IRON OXIDE ENCAPSULATED GOLD COLLOIDAL NANOPARTICLE VIA RAPID SONOCHEMICAL METHOD FOR MRI AND CT IMAGING APPLICATION

MOHAMMED ALI DHEYAB

UNIVERSITI SAINS MALAYSIA

2021

IRON OXIDE ENCAPSULATED GOLD COLLOIDAL NANOPARTICLE VIA RAPID SONOCHEMICAL METHOD FOR MRI AND CT IMAGING APPLICATION

by

MOHAMMED ALI DHEYAB

Thesis submitted in fulfilment of the requirements for the degree of Doctor of Philosophy

February 2021

ACKNOWLEDGEMENT

On this memorable day in my life, I reached the final destination of my journey as a PhD student; first of all, I would like to thank Almighty Allah for granting me health and patience to complete this research work.

Also, I am deeply thankful to my main supervisor, **Professor Dr. Azlan Abdul Aziz,** for his support, kind cooperation, useful contribution and valuable guidance throughout the course of this study. Thanks again, Prof. for having your door open every time I needed help.

I express appreciation to the staff of the Nano-Optoelectronics Research and Technology Laboratory (NOR lab) and Institute for Research in Molecular Medicine (INFORMM lab) assistants for technical assistance during my laboratory work, particularly in the sample characterizations.

My heartfelt gratitude also goes to my family members: to my father, mother, brothers, sisters and friends for their continuous prayers and support. Finally, I thank all who supported me in any respect during the completion of this study.

Mohammed Ali Dheyab

TABLE OF CONTENTS

ACKN	NOWLEE	OGEMENT	ii
TABL	E OF CC	DNTENTS	iii
LIST	OF TABI	LES	viii
LIST	OF FIGU	RES	ix
LIST	OF SYM	BOLS	xiv
LIST	OF ABBI	REVIATIONS	. xv
LIST	OF APPE	ENDICESx	viii
ABST	'RAK		xix
ABST	RACT		. xx
CHAI	PTER 1	INTRODUCTION	1
1.1	History o	f Nanotechnology	1
1.2	Iron Oxio	de Nanoparticles (Fe ₃ O ₄ NPs)	2
1.3	Core@sh	ell Nanoparticles (Fe ₃ O ₄ @Au NPs)	2
1.4	Problem	statement	3
1.5	Objective	e of the study	5
1.6	Scope of	the study	5
1.7	Contribu	tion of the study	6
1.8	Organiza	tion of the thesis	6
CHAI	PTER 2	LITERATURE REVIEW	7
2.1	A brief o	verview of iron oxide nanoparticles	7
2.2	Wet cher	nical methods for the synthesis of magnetite nanoparticles	7
	2.2.1	Co-precipitation method	8
	2.2.2	Electrochemical method	. 10
	2.2.3	Hydrothermal method	. 10
	2.2.4	Microemulsions and reverse micelles method	. 12

	2.2.5	Sol-gel method	14
	2.2.6	Solvothermal method	15
	2.2.7	Sonication method	16
	2.2.8	Thermal decomposition method	16
2.3	Surface	modification of Fe ₃ O ₄ NPs	21
	2.3.1	Inorganic coating	21
		2.3.1(a) Gold	21
		2.3.1(b) Silica	23
	2.3.2	Organic coating	24
		2.3.2(a) Chitosan	24
		2.3.2(b) Polyethylene Glycol (PEG)	25
		2.3.2(c) Polyvinyl Alcohol (PVA)	26
		2.3.2(d) Poly Vinyl Pyrrolidone (PVP)	27
2.4	Synthesi	is of Fe ₃ O ₄ /Au Core/shell nanoparticles	28
	2.4.1	Synthesis of a Fe ₃ O ₄ bi-layer structure	29
	2.4.2	Synthesis Fe ₃ O ₄ /glue/Au multilayer	32
2.5	Effect of	f sonochemistry on coating Fe ₃ O ₄ @Au core@shell NPs	36
2.6	The role	of Sodium Citrate	39
2.7	Fe ₃ O ₄ @	Au NPs for dual-mode MRI and CT scan	40
2.8	Summar	у	44
CHA	PTER 3	THEORETICAL BACKGROUND	45
3.1	Introduc	tion	45
3.2	Theory of	of sonochemistry	45
3.3	Cavitatio	on	46
3.4	Acoustic	c cavitation	47
3.5	Effects of	of cavitation	49
	3.5.1	Physical effect	49

	3.5.2	Chemical effect	50
	3.5.3	Thermal effect	51
3.6	Effects o	f Sonochemistry on stability	51
3.7	Magnetic	c properties of Fe ₃ O ₄ NPs	52
3.8	Ionic pro	perties of Au NPs	54
3.9	Response	e Surface Methodology (RSM)	55
3.10	Theory o	f Magnetic Resonance Imaging (MRI)	57
	3.10.1	T ₁ Relaxation Time	61
	3.10.2	T ₂ Relaxation Time	62
3.11	Theory o	f Computed Tomography (CT-Scan)	64
3.12	MRI and	CT-Scan Contrast Agent	65
3.13	Summar	у	68
CHA	PTER 4	METHODOLOGY AND OPTIMIZATION	69
4.1	Introduct	ion	69
4.2	Chemica	ls	69
4.3	Characte	rization	70
4.4	Synthesis	s of Fe ₃ O ₄ NPs	70
4.5	Synthesis	s of Au NPs using sonochemical method	73
4.6	Synthesis	s of Fe ₃ O ₄ @Au NPs	74
4.7	Model D	evelopment for Fe ₃ O ₄ Au NPs using sonochemical method	75
	4.7.1	Design of Experiment using RSM	75
	4.7.2	Significance of the independent variables of the Zeta potential for synthesised Fe ₃ O ₄ @Au NPs	77
4.8	Characte	rization of Fe ₃ O ₄ @Au NPs	78
	4.8.1	X-Ray Diffraction (XRD)	78
	4.8.2	Ultraviolet – visible spectroscopy (UV – vis)	81
	4.8.3	Transmission Electron Microscopy (TEM)	82
	4.8.4	Field emission scanning electron microscopy (FESEM)	84

	4.8.5	Energy dispersive x-ray (EDX)
	4.8.6	Zetasizer
	4.8.7	Vibrating Sample Magnetometer (VSM)90
4.9	The Fe ₃ O	D ₄ @Au concentration measurement91
4.10	The cyto	toxicity assay for Fe ₃ O ₄ and Fe ₃ O ₄ @Au92
4.11	Fe ₃ O ₄ @	Au for dual-mode MRI and CT scan94
4.12	Summar	y
CHA Fe3O4	PTER 5 @Au NPs	PHYSIOCHEMICAL PROPERTIES OF THE OPTIMIZED S AND THEIR MEDICAL APPLICATION
5.1	Introduct	tion
5.2	Response	e surface plots for Fe ₃ O ₄ @Au NPs97
5.3	Effect of	independent variables on zeta potential
5.4	Compari	son of predicted and experimental results 101
5.5	Physical	properties of Fe ₃ O ₄ @Au NPs 102
	5.5.1	X-Ray Diffraction (XRD) 102
	5.5.2	Ultraviolet-visible spectroscopy (UV-Vis)104
	5.5.3	Transmission electrons Microscope (TEM) analysis 106
	5.5.4	Field Emission Scanning Electron Microscopy (FESEM) Analysis
	5.5.5	Energy-dispersive X-ray Spectroscopy (EDX) Analysis 109
5.6	Materials	s stability of Fe ₃ O ₄ @Au110
5.7	Magnetic	c properties of Fe ₃ O ₄ @Au NPs112
5.8	The cyto	toxicity assay for Fe ₃ O ₄ and Fe ₃ O ₄ @Au in HEK-293 cells
5.9	Applicat	ions of Fe ₃ O ₄ @Au NPs for dual-mode MRI and CT scan 114
CHA	PTER 6	CONCLUSION AND FUTURE RECOMMENDATIONS 117
6.1	Conclusi	on117
6.2	Recomm	endations for Future Research

LIST OF PUBLICATIONS

LIST OF TABLES

Page

Table 2.1	Comparison between synthesis methods in preparation Fe ₃ O ₄ 19
Table 2.2	Comparison between various synthesis approach35
Table 2.3	Summary of the published articles on Fe ₃ O ₄ @Au core@shell NPs via sonochemical method
Table 2.4	Summary of the published articles on core@shell NPs43
Table 4.1	Experimental matrix76
Table 4.2	ANOVA results for zeta potential78
Table 5.1	Comparing the predicted and the experimental result101
Table 5.2	Comparison of size nanoparticles measured by TEM and FESEM.108
Table 5.3	Detailed elemental analysis of Fe ₃ O ₄ and Fe ₃ O ₄ @Au sample using
	EDX

LIST OF FIGURES

Page

Figure 2.1	Various methods of producing Fe ₃ O ₄ and its surface modifications with organic and inorganic materials
Figure 2.2	The formation of Fe_3O_4 NPs by mixing two water-in-oil microemulsions, where reactant 1 contains salt or a complex of a metal, while reactant 2 contains a precipitating agent [82]14
Figure 2.3	TEM images with different sizes and shapes of agglomerated Fe ₃ O ₄ depending on the method of synthesis (a) Co-precipitation [122] (b) Electrochemical [53] (c) Hydrothermal [62] (d) Microemulsion [70] (e) Sol-gel [123] (f) Solvothermal [91] (g) Sonication [124] (h) Thermal decomposition [125]18
Figure 2.4	Reaction steps of preparation Fe ₃ O ₄ /SiO ₂ core/shell nanoparticles by condensation and hydrolysis of sol-gel precursors like tetraethyl orthosilicate (TEOS) [147]
Figure 2.5	Schematic representation of two approaches for synthesis Au coated Fe ₃ O ₄
Figure 2.6	TEM images with different sizes and shapes of $Fe_3O_4@Au$ depending on the conditions of the synthesis method (a) Fe_3O_4/Au nanoparticles bi-layer [177], (b) $Fe_3O_4/PZS/Au$ [28], (c) $Fe_3O_4/PB/Au$ [188], (d) $Fe_3O_4/PANI/Au$ [194] and (e) $Fe_3O_4/PEI/Au$ [186] multilayer
Figure 3.1	Representation of sound frequency ranges, with a rough guide of some applications
Figure 3.2	Summary of the acoustic cavitation phenomenon steps that occur under ultrasonic radiation
Figure 3.3	Illustration of the mechanism of the sonochemistry treatment to break down the agglomerations of NPs

- Figure 3.6 Schematic illustration of relaxation procedure in the MRI. (1) The proton nuclei precess randomly (2) The total magnetic moment M of the spin aligns parallel to the external magnetic field. (3) A pulsed RF is introduced and (4) consequently, M_0 flip away from B to the XY plane. (5) When RF is tuned off, the spin diphase at a T_2 decay time and releases their absorbed energy, which is absorbed as MRI signal [278]......60
- Figure 3.8 Comparing MRI with and without contrast agents (a) image is without contrast (b) image is with contrast agent [291]......66
- Figure 3.9 Schematic representation of TE and TR [292]......66
- Figure 4.2 These experimental setups and equipment were used to produce Fe₃O₄@Au NPs.....74
- Figure 4.3 Photography displays different colours for as-synthesis (a) Fe₃O₄ NPs, (b) Au NPs and (c) Fe₃O₄@Au NPs......75

Figure 4.4	Bragg's diffraction for X-Ray diffraction by crystal plane79
Figure 4.5	XRD analysis of Fe ₃ O ₄ NPs [305]80
Figure 4.6	UV-vis result of Au NPs [306]81
Figure 4.7	Schematic diagram of 3600 spectrophotometer (Shimadzu) [307]82
Figure 4.8	The schematic diagram of transmission electron microscopy (TEM) system [308]
Figure 4.9	TEM image of Fe ₃ O ₄ @Au NPs with scale of 50 nm [188]84
Figure 4.10	SEM image shows the morphology of Fe ₃ O ₄ @Au NPs with scale of 1 μ m [35]85
Figure 4.11	Schematic diagram of FEI Nova NanoSEM [311]86
Figure 4.12	Schematic diagram of EDX- analyser [307]87
Figure 4.13	Schematic diagram of zeta potential for nanoparticles [316]89
Figure 4.14	Zeta potential results of Fe ₃ O ₄ @Au NPs [311]90
Figure 4.15	VSM analysis of Fe ₃ O ₄ at room temperature [317]91
Figure 4.16	Standard curve of the concentrations (a) iron and (b) gold92
Figure 4.17	Seeded HEK293 cells in a flat-bottomed 96-well plate (a) without Fe ₃ O ₄ NPs (b) with Fe ₃ O ₄ @Au NPs93
Figure 4.18	Enzyme-linked immunosorbent assay (ELISA)94
Figure 4.19	Agarose phantom mixed with different concentrations of Fe ₃ O ₄ @Au NPs For MRI and CT imaging95
Figure 5.1	Correlation between predicted and actual observed data from the 14 experimental results for zeta potential
Figure 5.2	Three-dimensional response surface and two-dimensional contour plots showing mutual interaction and individual effects of different variables on zeta potential of the synthesised Fe ₃ O ₄ @Au NPs (a, b) The response surface and contour plots of HAuCl ₄ (mL) vs SC (mL) while keeping sonication amplitude constant, (c, d) the response surface and contour plots of inoculum sonication amplitude vs HAuCl ₄ (mL) while keeping SC (mL), (e, f) the

response and contour plots of inoculum sonication amplitude vs SC (mL) while keeping HAuCl₄ (mL) constant......100

Figure 5.3	Optimized ramps show the optimized values of HAuCl ₄ , SC and
	sonication amplitude for improving the zeta potential of
	Fe ₃ O ₄ @Au NPs102
Figure 5.4	X-ray diffraction (XRD) patterns of (a) Fe_3O_4 and (b) $Fe_3O_4@Au$
	NPs104
Figure 5.5	UV-vis spectra of different colloidal suspensions (a) Fe ₃ O ₄ , (b) Au
	NPs and (c) Fe ₃ O ₄ @Au NPs105
Figure 5.6	TEM images and size distribution histograms of (a), (c) Fe_3O_4 and
	(b), (d) $Fe_3O_4@Au NPs107$
Figure 5.7	FESEM images and size distribution histograms of (a), (c) Fe ₃ O ₄
	and (b), (d) Fe ₃ O ₄ @Au NPs108
Figure 5.8	Energy-dispersive X-ray (EDX) of (a) Fe ₃ O ₄ @Au NPs and (b)
	Fe ₃ O ₄ 109
Figure 5.9	EDX mapping image of sample Fe ₃ O ₄ @Au NPs. The bright spots
	show the distribution elements of Fe, Au, C and O110
Figure 5.10	The stability measurement of as-synthesised nanoparticles using
	zeta potential (a) Fe ₃ O ₄ , (b) Au NPs and (c) Fe ₃ O ₄ @Au NPs112
Figure 5.11	(a) Magnetization curve of superparamagnetic (no coercivity nor
	remanence) Fe ₃ O ₄ @Au NPs at room temperature, the magnetic attraction of Fe ₃ O ₄ @Au NPs (b) Fe ₂ O ₄ @Au NPs in solution state
	(c) magnetic attraction of Fe_3O_4 @Au NPs towards a magnet
Figure 5.12	Biocompatibility test with different concentrations and incubation
	times (24, 48 and 72 h) (a) Fe ₃ O ₄ and (b) Fe ₃ O ₄ @Au NPs against
	the (HEK-293) cell line114
Figure 5.13	(a) T ₂ -weighted MR image with different Fe concentrations (0.1,
	0.2, 0.3, 0.4 and 0.5 mg). (b) The linear fitting of $1/T_2$ of the

 $Fe_3O_4@Au\ CNPs$ with different Fe concentrations. (c) CT image

of the Fe ₃ O ₄ @Au CNPs with different Au concentrations (1, 2, 3	3,
4 and 5 mg/ml). (d) x-ray attenuation intensity	116

LIST OF SYMBOLS

°C	Degree Celsius
Oe	Oersted (magnetizing field)
Нс	Coercivity
μl	Microliter
θ	Angle
λ	wavelength
ωο	Larmor frequency
ζ	Zeta potential
Bo	magnetic field
d _{hkl}	interplanar spacing
Dp	Crystal size
3	The strain
a	Lattice constant
h,k,l	Miller indices
γ	gyromagnetic ratio
Hz	Hertz
rpm	revolution per minutes
a.u	arbitrary unit

LIST OF ABBREVIATIONS

Mr	Remanence
Ms	Saturation magnetization
APTES	(3-Aminopropyl)triethoxysilane
VSM	A vibrating-sample magnetometer
СООН	Carboxylate group
T_2	Longitudinal Relaxation Time
r ₁	Transverse Relaxation rate
r ₂	Longitudinal Relaxation rate
DLS	Dynamic Light Scattering
TR	Repetition Time
TE	Echo time
T_1	Transverse Relaxation Time
ppm	parts per million
Fe ³⁺	Ferric
Fe ²⁺	Ferrous
FTIR	Fourier-Transform Infrared Spectroscopy
FeO(OH)	Goethite
a-Fe ₂ O ₃	Hematite
HCl	Hydrochloric acid
ОН	Hydroxyl group
Fe(acac) ₃	Iron acetylacetonate
IONPs	Iron oxide nanoparticles
Fe(CO)5	Iron pentacarbonyl
FeCl ₂	Iron(II) chloride

FeCl ₃	Iron(III) chloride
γ-Fe2O3	Maghemite
MNPs	Magnetic nanoparticles
MRI	Magnetic Resonance Imaging
СТ	Computed tomography
HU	Hounsfield Unit
NPs	Nanoparticles
Fe ₃ O ₄	Magnetite
Au	Gold
MW	Molecular Weight
O/W	Oil-in-Water
PDI	Polydispersity Index Values
PEG	Polyethylene glycol
PVP	Polyvinylpyrrolidone
pH	Potential of Hydrogen
RF	Radio Frequency
NaCl	Sodium chloride
NaOH	Sodium hydroxide
SPIONs	Superparamagnetic Iron Oxide Nanoparticles
TEM	Transmission Electron Microscopy
H ₂ O	Water
W/O	Water-in-Oil
XAFS	X-ray Absorption Fine Structure
XANES	X-ray Absorption Near Edge Structure
XRD	X-ray Diffraction
Adj. R2	Adjusted R – squared
Adeq. Pres.	Adequate precision

ANOVA	Analysis of variance
CCD	Central Composite Design
EDX	Energy-dispersive X-ray spectroscopy
FESEM	Field emission scanning electron microscopy
HAuCl ₄	Tetrachloroauric acid
HEK	Human embryonic kidney
NIR	Near-infra red
Pred. R2	Predicted R- squared
Prob.	Probability
RSM	Response Surface Methodology
SPR	Surface plasma resonance
UV-vis	Ultraviolet – visible spectroscopy
WST – 1	Water soluble tetrazolium - 1

LIST OF APPENDICES

- Appendix A1 T₂ weighted image of Fe₃O₄@Au NPs at TE 10 and TR 1000
- Appendix A2 T_2 weighted image of Fe₃O₄@Au NPs at TE 15 and TR 1000
- Appendix A3 T₂ weighted image of Fe₃O₄@Au NPs at TE 20 and TR 1000
- Appendix A4 T₂ weighted image of Fe₃O₄@Au NPs at TE 30 and TR 1000
- Appendix A5 T_2 weighted image of Fe₃O₄@Au NPs at TE 60 and TR 1000
- Appendix A6 T_2 weighted image of Fe₃O₄@Au NPs at TE 120 and TR 1000
- Appendix A7 T₂ weighted image of Fe₃O₄@Au NPs at TE 200 and TR 1000
- Appendix B CT image of Fe₃O₄@Au NPs at LEVEL: 40 HU, WINDOW: 120 HU

NANOPARTIKEL TERKAPSUL FERUM OKSIDA KOLOIDAL EMAS MELALUI KAEDAH SONOKIMIA PANTAS UNTUK APLIKASI MRI DAN PENGIMEJAN CT

ABSTRAK

Nanopartikel teras @ cengkerang (Fe₃O₄@Au NP) mempunyai pelbagai fungsi yang diperoleh dalam satu entiti stabil dan oleh itu telah diselidiki secara meluas. Walau bagaimanapun, kaedah langsung konvensional untuk sintesis Fe₃O₄@Au NPs sukar dan memakan masa. Oleh itu, kajian ini menyajikan teknik sonokimia yang mudah dan pantas untuk mensintesis Fe₃O₄@Au NP dengan sifat fizikokimia yang sangat baik untuk pengimejan resonans magnetik (MRI) dan imbasan tomografi terkomputer (CT). Potensi zeta sasaran - 46.125 mV dicapai dalam keadaan optimum 10 ml HAuCl₄, 30 ml SC dan amplitud sonikasi 40%, yang konsisten (sekitar 99.2%) dengan potensi zeta purata sebenar (- 45.8 mV). Kestabilan dan mono menyuraikan Fe₃O₄ NPs meningkat setelah pengubahsuaian menjadi Fe₃O₄@Au, seperti yang ditunjukkan oleh peningkatan potensi zeta dari – 24.2 mV menjadi – 45.8 mV. Nilai kemagnetan tepu (Ms) Fe₃O₄ adalah 54 emu / g, sementara nilai Fe₃O₄@Au NP adalah 38 emu/g. Fe₃O₄@Au NP menunjukkan keserasian bio yang baik dan potensi besar sebagai agen kontras mod dua untuk pencitraan MRI / CT. Nilai kelonggaran melintang dan pelemahan sinar-X dari NP yang disintesis (222,28 mM⁻¹ s⁻¹ dan HU = 418) lebih besar daripada nilai NP yang disediakan menggunakan kaedah konvensional dan NP komersial. Karya ini menunjukkan kemajuan yang cukup besar pada Fe₃O₄@Au NP dengan memberikan kaedah yang mudah dan pantas untuk mensintesis Fe₃O₄NPs bersalut Au berkualiti tinggi.

IRON OXIDE ENCAPSULATED GOLD COLLOIDAL NANOPARTICLE VIA RAPID SONOCHEMICAL METHOD FOR MRI AND CT IMAGING APPLICATION

ABSTRACT

Core@shell nanoparticles (Fe₃O₄@Au NPs) have multiple functions obtained in one stable entity and thus have been extensively investigated. Combining Fe₃O₄ and Au NPs in one core@shell nanostructure is a promising strategy for diagnostic biomedical applications. However, the conventional direct methods for Fe₃O₄@Au NPs synthesis are laborious and time-consuming. Therefore, this study presents a facile and rapid sonochemical technique of synthesising Fe₃O₄@Au NPs with excellent physicochemical properties for magnetic resonance imaging (MRI) and computed tomography (CT) scan. The Au shell is coated on Fe₃O₄ NPs using a Vibra-Cell ultrasonic solid horn with tip size, frequency and power output of ¹/₂ inch, 20 kHz and 750 watts, respectively within 10 minutes. The targeted zeta potential of - 46.125 mV was achieved under the optimum conditions of 10 ml of HAuCl₄, 30 ml of sodium citrate (SC) and sonication amplitude of 40%, which is consistent (about 99.2%) with the actual average zeta potential (- 45.8 mV). The stability and monodispersing of Fe₃O₄NPs improved following modification to Fe₃O₄@Au, as indicated by the increase in zeta potential from - 24.2 mV to - 45.8 mV. The saturation magnetization (Ms) value of Fe₃O₄ was 54 emu/g, while that of Fe₃O₄@Au NP is 38 emu/g. In general, the sonochemical method effectively synthesis highly stable and monodisperse Fe₃O₄@Au NPs with an average size of about 20 nm within 10 minutes. The Fe₃O₄@Au NPs showed good biocompatibility and great potential as a dual-mode contrast agent for MRI/CT imaging. The transverse relaxivity values and X-ray attenuation of the as-synthesised NPs (222.28 mM⁻¹ s⁻¹and HU = 418) are greater than those of NPs prepared using conventional methods and commercial NPs. This work reveals considerable progress on Fe₃O₄@Au NPs by providing a facile and rapid method to synthesise high-quality Au-coated Fe₃O₄ NPs. Importantly, the results demonstrate that all the objectives set for this thesis have been achieved.

CHAPTER 1

INTRODUCTION

1.1 History of Nanotechnology

The term "nanotechnology" was first introduced by Prof. Norio Taniguchi in 1974 [1]. However, the concept of "smallness" already evolved from its early inception when a Nobel Prize winner in Physics, Richard Feynman, presented the speech titled "There's Plenty of Room at the Bottom" at an American Physical Society meeting at Caltech in December 29, 1959 [2]. The presentation explored the prospect of directly manipulating discrete atoms as a more potent tool in chemical synthesis than the conventional approaches. Modern nanotechnology was launched with the manufacture of a scanning tunnelling microscope (STM), which is capable of visualizing individual atoms. According to the Oxford English Dictionary, nanotechnology is defined as "A branch of technology that focuses on tolerances and dimensions lower than 100 nanometres, particularly the manipulation of discrete atoms and molecules".

An intrinsic aspect of nanotechnology is that the physicochemical properties of nanoscaled materials varies highly from those of bulk materials with similar composition. For example, bulk gold material is recognized to be inert and unreactive as a catalyst, whereas gold nanoparticles exhibit a remarkably high catalytic reactivity in a wide array of reactions that include carbon monoxide and alcohol oxidation in the gas phase [3]. Another example for nanomaterials displaying differences in their properties from their bulk materials is non-magnetic bulk materials including Pt, Au and Pd nanomaterials embedded in polymer display magnetic moments at nanometric size of nanomaterials, whereas their bulk counterparts are non-magnetic [4, 5]. Two factors can attribute this variation in physicochemical properties reasons: (1) surface effect of the nanomaterials, where the fraction of atoms at the surface have fewer adjacent atoms compared to their bulk counterpart and (2) quantum effects that show discontinuous behaviour, which is attributable to the completion of shells in systems by delocalized electron [6]. Due to these distinctive properties, nanomaterials are extensively applied in many fields like electronics, energy, telecommunication and biomedical applications. The nanomaterials utilized for biomedical research and development applications comprise liposomes, polymeric micelles, block ionomer complexes, dendrimers, quantum dots and inorganic nanoparticles such as silica, gold and superparamagnetic iron oxide nanoparticles [7].

1.2 Iron Oxide Nanoparticles (Fe₃O₄ NPs)

Fe₃O₄ NPs are inorganic materials with diameters ranging from 1 to100 nm. Fe₃O₄ with a grain size of smaller than 20 nm display superparamagnetic behaviour (ability to have zero magnetism in the absence of external magnetic field) at high temperatures, since after the absence of the magnetic field, their magnetization will disappear, thus preventing the possible agglomeration and embolization of the capillary vessels [8]. Furthermore, these particles exhibit no coercivity and remanence at room temperature [9, 10]. Fe₃O₄ NPs are extensively utilized in several biomedical applications such as Magnetic Resonance Imaging (MRI), Computed Tomography (CT), drug delivery, biosensors, and hyperthermia [11]. The use of Fe₃O₄ nanoparticles in these applications is based on their relatively low toxicity, slow oxidation, high saturation magnetization, and higher magnetic susceptibility compared to maghemite (γ -Fe₂O₃) [12].

1.3 Core@shell Nanoparticles (Fe₃O₄@Au NPs)

Surface modification of Fe_3O_4 NPs with a suitable shell is a necessary action for the various application of Fe_3O_4 for two reasons: (i) being nanometer sizes, the ratio of the surface to volume makes them highly active which require surface modification to minimize the surface energy for keeping the appropriate chemical stability, (ii) the advantages of Fe_3O_4 NPs become available only when it is well dispersed in the solution; therefore, the modification is effective to prevent the agglomeration. Au shell is considered the most viable option for fabricating magnetic core@shell NPs because it is biocompatible, chemically stable, and possesses exceptional optical characteristics and non-complex biofunctionalization. The rapid magnetic responsiveness of the magnetic core and exceptional biocompatibility of Au shell enable conjugation with relevant biomolecules as well as ensure their applicability in the biomedical field [13-18].

1.4 Problem statement

Numerous methodologies have been employed to synthesise Fe₃O₄ core coated with Au shell. One example is a direct coating, which is simple but involves a difficult process of combining two seemingly incompatible surfaces. The results usually indicate poor dispersion and thus fail to produce Fe₃O₄@Au NPs [19]. Additionally, the process is laborious and time-consuming [20], hindering the irregular shape and also the size of more than 100 nm, resulting in an undesired effect on their biomedical applications [21]. The efficacy of the nanoparticles for biomedical application depends on their stability and biocompatibility [22]. The stability of the NPs and consequently, their nanoscale size is also paramount for their elimination/excretion out of the organism after the diagnostic. Hence, to reach and pass clinical tests with NPs, the right choice of the coating matters because this ultimately enables NPs to fulfil their task in the complex environment of biological fluids, cells and organisms [23]. In addition, the toxicity of NPs has been shown to be dependent on their stability [24],

which has also led to a need to understand the behaviour of NPs suspensions to be settled. Importantly, the nanoparticles, which change particle stability over time, could potentially cause toxic effects [25]. A few studies have been reported for synthesis Fe₃O₄@AuNPs using a sonochemical method but still, there is a lack of stability measurement as well as the use of Fe₃O₄@AuNPs for medical applications that sonochemically synthesised [26-28]. In addition, modern optimization protocols (individually) are unable to predict the relationship between variables and timeconsuming procedures requiring multiple experiments and the use of toxic chemicals [29]. The advantage of the response surface methodology (RSM) is its ability to handle variables (HAuCl₄, sodium citrate (SC), and sonication amplitude) and response (zeta potential) without the limitations mentioned above [30], this enables the development of an appropriate predictive model capable of correlating responses to multiple factors, even in cases of complex interactions [31]. Despite the numerous applications by RSM for the optimization of experimental procedures [32-35], this study is the first to combine RSM with zeta potential to systematically investigate the influence of the sonochemical effect on the surface functionalization process.

In this research, a rapid and simple sonochemical approach was explored to synthesise Fe₃O₄@AuNPs with unique physiochemical features such as good monodispersed, uniformity, stability, biocompatibility and potential application as a dual-mode contrast agent for MRI and CT imaging in a short time. Therefore, this work was also aimed to optimize the sonochemical conditions for the effective Au coating of Fe₃O₄ core NPs for the synthesis of highly stable Fe₃O₄@Au NPs via a sonochemical approach. Using RSM, various parameters were used to optimize the zeta potential value of as-synthesised Fe₃O₄@Au NPs such as gold precursor, sodium citrate and the sonication amplitude. One parameter was fixed at its optimum level for

a single run, whereas the other two parameters were varied within their experimental ranges.

1.5 Objective of the study

The main objectives of this report are summarized in the points below:

- To synthesis a highly stable Fe₃O₄@AuNPs using sonochemical method in a short time.
- **2.** To optimize the synthesised $Fe_3O_4@AuNPs$ via RSM and investigate the interaction effects among the independent variables on response.
- **3.** To evaluate the physicochemical properties and their toxicity of Fe_3O_4 and $Fe_3O_4@Au$.
- 4. To evaluate the sensitivity of the Fe₃O₄@Au NPs prepared under optimum synthesis parameters for application as a dual-mode contrast agent for MRI and CT imaging.

1.6 Scope of the study

The scope of this study is limited the preparation of Fe₃O₄ core coated with Au shell to generate highly stable Fe₃O₄@AuNPs using a sonochemical method in a short time. The optimization process was based only on response surface methodology (RSM). The frequency/power of the ultrasonic probe is limited to 20 kHz/750 watts in 10 minutes. MRI and CT used only agar phantom with Fe₃O₄@AuNPs as a dual-mode contrast agent.

1.7 Contribution of the study

This study contributes on the new knowledge about a rapid and simple sonochemical approach to synthesise Fe₃O₄@AuNPs with high stability and biocompatibility acting as a dual-mode contrast agent for MRI and CT imaging in a short time.

This study also contributes to the subject of optimizing the sonochemical conditions for the effective Au coating of Fe₃O₄ core NPs using RSM.

1.8 Organization of the thesis

This thesis comprises of six chapters. The introduction, problem statement, objectives and aims of this thesis are presented in Chapter 1. Literature review on synthesis of Fe₃O₄, Fe₃O₄@AuNPs and surface modification with different organic and inorganic are presented in Chapter 2. The various theories used to support this research are presented in Chapter 3. The whole experimental procedures, characterisation techniques and optimization of the as-synthesised Fe₃O₄@AuNPs for application as a dual-mode contrast agent for MRI and CT imaging are described in chapter 4. Details of the various results observed in this work are highlighted and discussed in Chapter 5. The conclusion and future work of this thesis is presented in Chapter 6.

CHAPTER 2

LITERATURE REVIEW

2.1 A brief overview of iron oxide nanoparticles

In recent times, magnetite nanoparticles (Fe₃O₄ NPs) have been comprehensively researched because of their extensive biomedical uses, e.g. cancer treatment, drug delivery, hyperthermia therapy and dual-mode contrast agent for MRI and CT scan. Fe₃O₄ NPs (≤ 20 nm) possess exceptional properties that include biocompatibility, non-toxicity, good magnetic susceptibility and superparamagnetic behaviour [9, 36]. Superparamagnetic behaviour is an essential characteristic of Fe₃O₄, since, after the absence of an external magnetic field that applies to Fe₃O₄, their magnetization will disappear (zero magnetism), preventing the possible agglomeration and embolization of capillary vessels [8].

2.2 Wet chemical methods for the synthesis of magnetite nanoparticles

There are several widely reported chemical methods for the synthesis of Fe₃O₄ nanoparticles for biomedical applications, namely co-precipitation, electrochemical, hydrothermal, microemulsions and reverse micelles, sol-gel, solvothermal, sonication and thermal decomposition. In general, all agree that the synthesis of Fe₃O₄ nanoparticles is a complicated process due to their colloidal nature. The advantages, disadvantages, and features of the obtained Fe₃O₄ products from each method are summarized in Table 2.1. These methods' main challenges consist of determining the experimental conditions for synthesising monodisperse of Fe₃O₄ grains with the desired size. These chemicals methods have been successfully employed to synthesis nanoparticles with narrow size distribution and homogeneous composition. Figure 2.1

shows extensive synthesis methods of Fe_3O_4 nanoparticles along with its surface modifications.



Figure 2.1 Various methods of producing Fe₃O₄ and its surface modifications with organic and inorganic materials

2.2.1 Co-precipitation method

The co-precipitation method is one of the most important and common chemical wet methods for the preparation of Fe₃O₄ in addition to controlling the size and shape of the aqueous solution because its unique features, which include simplicity, ability to be up scaled to a large-scale production, ability to synthesize hydrophilic compounds, and the possibility of being performed at room temperatures [37]. It is also the simplest chemical reaction to produce superparamagnetic iron oxide nanoparticles, SPIONs [38]. A strong base solution such as NaOH, NH4OH and KOH are added to the solution to facilitate the chemical process at room temperature [39], while a weak base such as Na₂CO₃ is used for a very slow reaction [40]. The preparation of Fe₃O₄ via the co-precipitation method involves the reaction between ferric and ferrous with at ratio 2:1 or 1:1 with vigorous stirring in an aqueous media [41]. The type of precipitating agent

plays a significant role in determining the physicochemical and magnetic properties of Fe₃O₄ nanoparticles [42]. When strong alkaline media such as LiOH, KOH, and NaOH are used as hydrolyzing agents, an impurity such as Goethite (α FeO(OH)) is observed but virtually absent when ammonia (NH₃) is utilized [43]. The impurity affects and contributes to a decrease in the particles' magnetic moment [44]. Several organic materials served as a peptizing agent in Fe₃O₄ nanoparticle syntheses such as a Citric acid (C₆H₈O₇), nitric acid (HNO₃), perchloric acid (HCI₄), and tetramethylammonium hydroxide (C₄H₁₃NO) to prevent agglomeration of Fe₃O₄ nanoparticles by electrostatic repulsion [45]. Eventually, these substances are incompatible with biomedical applications because they possess an unacceptable percentage of toxicity.

Previous studies have shown that the size of Fe_3O_4 particles can be controlled by adjusting the reaction conditions such as reaction time, the ratio of concentration Fe^{2+}/Fe^{3+} , pH, temperature, ionic strength in the medium and stirring speed [45, 46]. The saturation magnetization is directly proportional to the size of the Fe_3O_4 where the magnetism will decrease when the particle size is small [47]. The main drawbacks of the co-precipitation method are the agglomeration and polydisperse of Fe_3O_4 nanoparticles. However, recently many researchers have revealed that polymers' presence in chemical reactions can assist a successful synthesis of highly monodisperse and non-agglomeration Fe_3O_4 particles via steric repulsion [48, 49]. In other words, the polymer works to separate the nucleation and growth process as a capping agent and prevents growth after the process of nucleation. The co-precipitation used NaOH can be easily implemented and requires less time and has the highest yield. Nonetheless, the same cannot be said about when NH₃.H₂O is used. Results show that smaller size and low output yield were obtained, and longer synthesis time was required [50]. During the preparation process, it is preferable to have an N₂ gas to protect the product from oxidation with the desired temperature. At the end of the process, according to previous studies, a quick visual indicator for good Fe₃O₄ is black [51].

2.2.2 Electrochemical method

The electrochemical process of producing superparamagnetic iron oxide nanoparticles (SPIONs) is based on oxidation and reduction reaction of iron which base electrolyte's in an electrolyte. The electrochemical method has also been utilized to generate various Fe_3O_4 nanoparticles phases such as magnetite (Fe_3O_4) and maghemite (Fe_2O_3) nanoparticles [52]. This phenomenon can be explained by crossing an electric current through two electrodes (anode and cathode). More so, the positively charged electrode (anode) can be oxidized to metal ion species inside the electrolyte and the metal ion is later reduced to metal by the negatively charged electrode (cathode) with the assistance of stabilizers. The Fe_3O_4 nanoparticles are generally deposited on the electrode generally in a coating or thin film. The synthesis of Fe_3O_4 nanoparticles via this method does not require high temperature and the electrolyte's temperature must be less than the boiling point. This method has a disadvantage at room temperature, often produces poorly ordered particles that cause an explicit structural characterization hard [53].

2.2.3 Hydrothermal method

A hydrothermal method is one of the most common wet chemical ways for the synthesis of inorganic nanocrystals, especially for metal and metal oxides [54, 55]. The formation of Fe_3O_4 nanoparticles involves two steps; firstly, the hydrolysis reaction, and then the dehydration process, as demonstrated in Equation (1) and (2) [56].

$$Hydrolysis: M^{n+} nH_2 0 \rightarrow M(OH)_n + nH^+$$
(2.1)

Dehydration:
$$M(OH)_n \rightarrow MO_{n/2} + {}_{n/2}H^+$$
 (2.2)

This method often utilizes relatively high temperature and pressure to influence the formation of nanocrystals. It includes the heating of a water solution of iron salt at a temperature and pressure of 374 ° C and 22.1 MPa, respectively. The hydrothermal process has various advantages such as facile control, environmentally friendly process, good crystallization and morphology of products. In addition, under this high pressure, some metastable and condensed phases can be produced. Different shapes of Fe₃O₄NPs have been prepared via hydrothermal syntheses, such as nanorods, nanowires, nanospheres amd many other shapes [57-59]. Fe₃O₄ nanoparticles with an average of 50 nm have been prepared by utilizing Na₂S₂O₃ as the control agent via the hydrothermal method.

The synthesising of the Fe₃O₄ nanoparticles phase depends on the ratio of Na₂SO₃ to FeSO₄ [60]. Fe₃O₄ nanoparticles with size 27 nm in the presence of a suitable surfactant via hydrothermal process have been prepared [61]. Previous studies demonstrated that microwave hydrothermal with a temperature range of 90 to 200°C had demonstrated spherical Fe₃O₄ nanoparticles with sizes ranging between 150-200 nm by using the FeCl₃.FeSO₄.7H₂O as precursors and NaOH as hydrolysis reactant. It was found the formation of Fe₃O₄ nanoparticles controlled by a critical parameter (Fe/NaOH). Chen et al. reported that Fe₃O₄ nano-powders prepared via a hydrothermal process by employ Fe²⁺ precursor (FeCl₂·4H₂O). They used the FeCl₂ to react with the mixing of N₂H₄ and NaOH; thus, the iron salts Fe²⁺ and Fe³⁺ had partially oxidized by N₂H₄[62].

The hydrothermal method also used the Polyvinylpyrrolidone (PVP) as the surfactant where the shape of Fe₃O₄ nanoparticles can be controlled by mixing FeSO₄.7H₂O, NaOH, FeCl₃ with benzene and PVP. By varying PVP amount and

experimental conditions, Fe₃O₄ nanoparticles with different morphologies can be obtained, like nanowires, nanorods, nanoparticles and mixtures [63]. However, the disadvantage of this method is the slow reaction kinetics at any proposed temperature. Therefore, microwaves assisted hydrothermal process was proposed [64]. The microwave heating process provides increased interaction kinetics and improved crystallization of the sample. By combining of two process hydrothermal effects and microwave irradiation, the morphology of synthesised SPIONs can be adjusted or controlled. SPIONs with cubical shaped or rhombohedral, hexagonal were reported [65]. In this study, the hydrothermal method recorded many advantages features such as high yield, controllable size, excellent particle crystallinity and good morphology [66].

2.2.4 Microemulsions and reverse micelles method

A stable or thermodynamically stable system consists of two liquids immiscible such as oil and water in addition to the presence of surfactant aggregate [66]. There are three types of microemulsions; firstly, direct oil in water microemulsion (o/w), secondly, reversed water in oil (w/o), and thirdly, bicontinuous. This classification depends on the hydrophilic-lipophilic balanced value and water ratio to oil (w/o) [67]. Nanoparticles formation under the microemulsion method undergoes four phases. I), mixing of microemulsion components II), exchange of substances through the nanodroplets, III) reaction nucleation and IV), reaction outgrowth [68]. Particle stability via this method is influenced by the amount and type of surfactant, and the pH of the dispersing medium [69].

As demonstrated in Figure 2.2, when two nanoparticles collided together, the reactants would be exchanged for the formation of nanoparticles by the Brownian movement [70]. A water droplet covered with a suitable surfactant is called a

nanoreactor. More importantly, the surfactant prevents water droplets from forming excess aggregation [71]. A study has recently demonstrated that the microemulsion process can synthesis monodisperse SPIONs by varying the concentration of precursor and size of the droplet radius, as shown in Figure 2.3d [72]. SPIONs can be prepared through two methods firstly, water in oil (w/o) and the second oil in water (o/w) via microemulsions process [73]. The conventional method of synthesis SPIONs via microemulsion need to add reducing agent such as ammonia to reactants [74]. The size distribution and shape can be controlled by manipulation in the amount of surfactant, water and oil via microemulsion process [75], while using different temperatures during the reaction produced Fe₃O₄ nanoparticles with a diameter in the range of 3 to 12 nm [76]. Jia et al. reported a new procedure by adding basic solution NaOH as a reducing agent to produce Fe₃O₄ surrounded by chitosan. This component's size ranged from 10-80 nm [77]. Like the problem observed in the co-precipitation method, the main disadvantage is the agglomeration and inability to monodispersed the particles and precisely control the size. Furthermore, a large amount of dissolvent is necessary to synthesis a ratable amount of nano-materials and to reverse the effects of residual surfactants on the property of the particles [78]. In order to overcome those limitations, oleic acid can be added to the reactants as stabilizing agents [79]. This method's main advantage is that it is environmentally friendly and economical [80]. More importantly, the SPIONs synthesised via this method depends on droplet size, surfactant and the concentration of reactant [81].



Figure 2.2 The formation of Fe_3O_4 NPs by mixing two water-in-oil microemulsions, where reactant 1 contains salt or a complex of a metal, while reactant 2 contains a precipitating agent [82]

2.2.5 Sol-gel method

In wet chemical approaches, sol-gel is one technique for producing Fe₃O₄ nanoparticles with unique properties, which involves hydroxylation and condensation of precursors turn into an inorganic solid [83]. Fe₃O₄, prepared via sol-gel, is very high purity and homogeneous [84]. The morphology and structure can be adjusted by adjusting the parameter, such as the salt precursors' concentration, pH, agitation, and temperature [85]. However, the change in pH also affects the magnetic properties of the resulting materials [86]. There are four steps in synthesising Fe₃O₄ nanoparticles using this method; (a) hydrolysis and poly-condensation of iron precursor in a solvent to form a colloidal suspension of the particles (sol), (b) gelation of the sol to form a gel, (c) the aging and (d) drying of the particles. Nevertheless, similar to the co-precipitation process, the sol-gel is challenged to produce monodisperse particles and prevent agglomeration. Several improvements have been reported to the synthesis of

monodisperse and non-agglomerated via the sol-gel process to overcome both limitations. Dong and Zhu. have been recorded that polyethylene glycol (PEG) can be used as a capping agent to mitigate the agglomeration and give the uniform size of Fe₃O₄ nanoparticles [87]. The sol-gel method has been prepared to synthesis nanocomposite materials by using aqueous methods [88]. The method used in this study has several merits. Firstly, its ability to monitor the fine structure identity of the reaction outputs. Secondly, its ability to get a pure amorphous stage, solo-dispersity, and well monitoring of the particle diameter. Thirdly, it is possible to get items with a prearranged shell regarding empirical situations.

2.2.6 Solvothermal method

A solvothermal method involves presenting the organic solvent like ethanol, methanol or polyol at an extremely high temperature and pressure [89]. Recently, many authors demonstrated that SPIONs had been synthesised by a solvent such as hydrazine (N₂H₄) and ethylenediamine (C₂H₈N₂) [90, 91]. The morphology and good uniformity in this method result from the reaction between the iron precursor and surfactant [92]. J. Liang et al. have been demonstrated that the size of Fe₃O₄ nanoparticles can be controlled by changing the ratio of surfactant, the concentration of NaOH, and precipitator [93]. In the solvothermal technique, the dispersity of iron salts, the temperature of reaction and the aging time are crucial parameters in determining the size distribution and controlling the nucleation and growth processes [94, 95]. Various surfactants such as sodium dodecyl benzene sulfonic, polyacrylic acid [93], and oleic acid [96] have been utilized as capping agents to preparation Fe₃O₄ nanoparticles with high monodispersity. The Fe₃O₄ nanoparticles that were prepared by this method are hydrophilic, which can be dispersed in an aqueous solution or polar solvents [97]. This method's advantages include no requirement for any surfactant or reducing agents except liquid polyols and control experimental conditions [98].

2.2.7 Sonication method

Sonication method (sonochemical or sonolysis) is a facile way to synthesis SPIONs and other nanostructure by decomposition (sonolysis) of an inorganic iron precursor using very high temperature and pressure generated by ultrasonic irradiation, up to 5000 K and 1000 atm, respectively [99]. The ultrasonic irradiation produces high temperature leads to generates magnetic nanoparticles by decomposition iron salts [100]. Hydrophilic and monodisperse properties of SPIONs have been improved via sonication method [101]. Recently, many authors reported the presence of a suitable stabilizer to contribute to synthesis SPIONs with high dispersed via ultrasonic irradiation [102, 103]. The sonication method often produces an amorphous shape because of the high temperature and pressure resulting from this process [104, 105]. More importantly, during the formation process of SPIONs, the acoustic cavitation process inhibits crystallization. More so, the crystalline properties of the SPIONs can be controlled by heat treatment [105].

The synthesising of SPIONs with crystalline properties at low ultrasonic temperature also has been recorded [106]. Sonication method for synthesising Fe_3O_4 NPs depends on a number of parameters, such as temperature, time, sonication frequency, to control size distributions and morphology [105].

2.2.8 Thermal decomposition method

The thermal decomposition technique is a well-known process for synthesising monodisperse and highly crystalline of SPIONs [107]. It involves the decomposition of iron precursors by very high temperatures [108]. In addition, the crystallinity and

magnetic properties of SPIONs can be obtained by increasing the mixture reaction up to 300°C [109]. During the thermal decomposition process, the nanoparticles undergo two important routes for control nucleation and growth mechanization. Firstly, involve direct injection of organometallic compounds in hot surfactant solution that results in the immediate formation of nuclei. Secondly, involves control heating of these compounds in surfactant solution for nuclei formation [110]. Park et al., Roca et al. and Baaziz et al. have reported that the precursor concentrations and the ratio of Fe/oleic acid are as critical parameters in controlling nanoparticles size [111-113]. A hightemperature reaction of Fe₂O₃ acetylacetonate with 1,2-hexadecanediol in existence oleylamine and oleic acid is needed to acquire monodisperse magnetite nanoparticles. In presence of a bipolar surfactant, the hydrophobic nanoparticles can be converted into hydrophilic and the diameter of particles also tuned from 4-20 nm [114]. N.R. Jana et al and M. Mohapatra et al have been proposed the use of non-toxic FeCl₃ and FeCl₂ salts as a precursor [115, 116].

Recently, the thermal decomposition method producing a water-dispersible magnetic nanoparticle in acidic has been synthesised using FeCl₃ and Fe(acac)₃ [117]. The diameters nanoparticles of 4,12 and 60 nm can be controlled according to the time of reflux (condensation of vapours and the return of this condensate to the system) [118]. Interestingly, the shape of nanoparticles from spherical to cubic has been changed by increasing reflux time. The synthesis of Fe₃O₄ via thermal decomposition method requires further investigation on the mechanism of chemical conversions because the reaction mixtures produced contain multicomponent reactions e.g., different kind of components was produced during the oxidative of Fe (II) including iron Fe₃O₄, γ - Fe₂O₃, FeO, (α -Fe), α -Fe₂O₃, siderite (FeCO₃) and iron carbide(Fe₃C) [119]. The advantages of thermal decomposition are inexpensive iron-organic precursors and very short

reaction time. Thermal decomposition process also has some disadvantages such as complicated procedures [89], emission of toxic gases such CO [120], uses toxic and expensive reagents (not environmentally friendly) [82], required high reaction temperature [89], uses the multiple reagents [89] and the inability to get required nanoparticle size [121]. Future development of this method should strive towards the synthesis of water-soluble magnetic nanoparticles directly that uses less reagents.



Figure 2.3 TEM images with different sizes and shapes of agglomerated Fe₃O₄ depending on the method of synthesis (a) Co-precipitation [122] (b) Electrochemical [53] (c) Hydrothermal [62] (d) Microemulsion [70] (e) Sol-gel [123] (f) Solvothermal [91] (g) Sonication [124] (h) Thermal decomposition [125]

Table 2.1	Comparison	between synthesi	s methods in n	reparation $\text{Fe}_{2}\Omega_{4}$
1 auto 2.1	Comparison	between synthesi	s memous m p	10paration 1 0304

Method	Features of the obtained Fe ₃ O ₄ products	Reaction condition	Advantage	Disadvantage	Yield	Ref.
Co-precipitation	Magnetization value: 20-80 emu/g Size distribution: Broad Shape control: Not good	Temperature: 20- 90°C Duration: Minutes	Facile, simple, easy, low cost and controllable size.	Agglomeration and difficulty in avoiding nucleation during the reaction	High	[126]
Electrochemical	Magnetization value: 35.5 emu/g Size distribution: Medium Shape control: Medium	Temperature: Room temp Duration: Hours- days	Facile, high purity and particle size can be controlled	Complex procedure	Medium	[53]
Hydrothermal	Magnetization value: 20-80 emu/g Size distribution: Very narrow / Narrow-broad Shape control: Very good	Temperature: 150- 220°C Duration: Hours- days	Facile, crystalline, highly pure and environmentally friendly	The crystal growth cannot be controlled	High	[127]
Microemulsions	Magnetization value: up to 113 emu/g Size distribution: Narrow Shape control: Good	Temperature:20-50°CDuration: Hours	Uniform and thermodynamically stable nanoparticles	Complex and heterogeneous	Low	[73]
Sol-gel	Magnetization value: 10-40 emu/g	Temperature:25-200°CDuration: Hours	Desired shape and hybrid nanoparticles	The product contains a sol-gel mixture component	Medium	[128]

	Size distribution: Narrow Shape control: Good					
Solvothermal	Magnetization value: up to 108 emu/g Size distribution: Narrow-broad Shape control: Good	Temperature: 150- 220°C Duration: Hours- days	High Purity, good crystallinity	Relatively slow kinetic and sensitive to the concentrations of alkalinity and water	High	[92]
Sonication	Magnetization value: 63 emu/g Size distribution: Narrow Shape control: Bad	Temperature: 20- 50°C Duration: Minutes	Facile, rapid and environmental friendly	Amorphous nanoparticles	Medium	[129]
Thermal decomposition	Magnetization value: up to 91 emu/g Size distribution: Very narrow Shape control: Very good	Temperature: 100- 320°C Duration: Hours- days	Monodispersed, inexpensive and high quality of Fe ₃ O ₄ nanoparticles	Complicated and requiring high temperatures	High	[130]

2.3 Surface modification of Fe₃O₄ NPs

The modification of Fe₃O₄ nanoparticles surface with organic or inorganic materials can provide biocompatible nanoparticles for biomedical application. Coating Fe₃O₄ nanoparticles with inorganic materials such as gold and silica nanoparticles gave them many advantages, including high stability and the ability to bind biological molecules to Fe₃O₄ nanoparticles' surface. On the other hand, if hydrophobic Fe₃O₄ nanoparticles are coated with organic materials (hydrophilic polymers) such as chitosan. Polyethylene glycol (PEG), Polyvinyl Alcohol (PVA), and Polyvinylpyrrolidone (PVP), the agglomeration of the iron oxide nanoparticles can mostly be avoided.

2.3.1 Inorganic coating

2.3.1(a) Gold

Gold is an inorganic coating to implement functionality and improve the stability of magnetic nanoparticles in aqueous dispersions. Au coating has a unique feature called surface plasmon resonance (SPR) which provides optical properties. Besides, the coating with Au nanoparticles can also promote organic conjugation via Au-S chemistry. Fe₃O₄ coated with Au has been reported by several authors [131, 132]. The coating process is obtained by reducing the Au precursor in the existence of iron oxide nanoparticles. The experimental conditions differ according to the Fe₃O₄ nanoparticle characteristics like size, shape, surface chemistry and the solubility, etc. Here we introduce some brief examples.

Xu et al. reported that magnetic Fe_3O_4/Au core/shell nanoparticles can be synthesised by reducing HAuCl₄ at room temperature. However, the work also indicates that the coating process of Au nanoparticles to cover the surface of Fe_3O_4 is difficult because of the incompatible chemistry involved. Furthermore, the rapid reduction of HAuCl₄ will lead to Au nanoparticles' growth rather than of a coating shell. To prevent the rapid reduction, the process utilizes oleylamine as a moderate reduction agent in a chloroform solution to slowly reduce HAuCl₄ of Fe₃O₄ nanoparticles. Additionally, chloroform is a strong solvent and uses as a surfactant that may help the desorption of oleylamine from the surface of Fe₃O₄ nanoparticles. Fe₃O₄/Au core/shell nanoparticles were soluble in a nonpolar solvent due to an oleylamine still capped at the surface. To make Fe₃O₄/Au water-soluble, Fe₃O₄/Au core/shell nanoparticles were dried and mixed with cetyltrimethylammonium bromide (CTAB) and sodium citrate. The negative charge on the Au nanoshell surface is due to the surface that may absorb the sodium citrate, which further led double-layer structure with the capping CTAB and a powerful capping can be achieved to replace oleylamine. Under the reducing condition, the shell thickness Au depends on the ratio of HAuCl₄. This method not only protects Fe₃O₄ from environmental corrosion but also able to manipulate and improve the SPR properties of the core/shell nanoparticles [132].

Zhong et al. reported another method to synthesis Fe₃O₄/Au core/shell [133]. The method includes Au (Ac)₃ as a precursor with temperature ranged 180-190°C in the existence of Fe₃O₄ nanoparticles, which used the reducing agent such as 1,2-hexadecandediol and surfactants like oleylamine and oleic acid. At high heating temperature, the adsorption process of oleic acid and oleylamine is facilitated from Fe₃O₄ nanoparticles' surface. This method employed a centrifuge to select the proper size and separated the small-sized and large-sized core/shell nanoparticles and uncoated Fe₃O₄ nanoparticles. In addition, this method can control a combination of thermally activated desorption of the capping layer and deposition of Au on the bare Fe₃O₄ surface, and re-encapsulation of the Au surface by the capping agent. The shell

thickness of Au nanoparticles was determined by TEM analysis [134]. After coating, the thiol inter-particle was used to produce thin Fe₃O₄/Au core/shell nanoparticles.

2.3.1(b) Silica

Silica (SiO₂) has been employed as an inorganic coating material for nanoparticle surface modification in the colloid system [135]. Usually, the silica shell over Fe₃O₄ nanoparticles' surface provides protection against toxicity, prevents the aggregation of Fe₃O₄ nanoparticles in liquid, and improves the chemical stability [136]. There are two different ways for the stability of silica coatings over Fe₃O₄ nanoparticles [137]. Firstly, protection of the dipole interaction with the silica shell and secondly since silica is negatively charged so it enhances the Coulomb repulsion of Fe₃O₄. The product is formed of Fe₃O₄ particles coated with silicon and its diameter 300 nm has been examined in the clinic by oral administration, they found it extremely improves the diagnosis of organ boundaries, like lymph nodes and uterus [138, 139].

Three strategies to create magnetic silica nanospheres will be presented. The first strategy depended on the famous Stöber process, which states silica was produced in situ by condensation and hydrolysis of sol-gel precursors like tetraethyl orthosilicate (TEOS) (Figure 2.4) [140]. Xiong et al. have recorded silica colloids filled with SPIONs by this process have been recorded [141]. This study revealed that there are two key factors to determine the final size of the silica colloids type of solvent and the other is the concentration of Fe₃O₄ nanoparticles. The second strategy implicates a deposition of silica from the silicic acid solution [142]. Several researchers have demonstrated the silica acid seems to be more effective than TEOS method in covering the Fe₃O₄ surface [143]. This method is easy and the particle size can be controlled by varying the ratio of Fe₃O₄ or SiO₂ [144]. The third strategy was about an emulsion way, in which micelle or inverse micelle is used to limit and control the coating of silica wherein the separation

of core/shell nanoparticles from the surfactant is associated with an emulsion system [145]. For instance, Yang et al. have employed this technique in the preparation of silica-coated SPIONs with monodisperse and increased the entrapment of biological molecules in the nanoparticles [138].

Tartaj et al. used a pyrolysis method for coating magnetic sphere aerosol by silica [146]. Gao et al. used seeds hydrophilic Fe_3O_4 nanoparticles with size 20 nm used to prepare Fe_3O_4/SiO_2 core/shell nanoparticles and the thickness of a SiO₂ shell may be tuned from 12.5-45 nm by varying the experimental conditions.



Figure 2.4 Reaction steps of preparation Fe₃O₄/SiO₂ core/shell nanoparticles by condensation and hydrolysis of sol-gel precursors like tetraethyl orthosilicate (TEOS) [147]

2.3.2 Organic coating

2.3.2(a) Chitosan

Chitosan is a biopolymer that has immense structural opportunities for mechanical and chemical modifications to produce novel features, application and functions, especially in the biomedical section. It is hydrophilic, non-toxic, non-antigenic, biodegradable and biocompatible polymer [148]. These days, the synthesising of Fe_3O_4 NPs encapsulated within chitosan are of paramount importance [149]. The presence of hydroxyl and amino on the chitosan would quickly form complexes with Fe_3O_4 surface and make them stable, hydrophilic and biocompatible.

The positive charge of amino groups could interact with a negative charge of nucleic acids for MRI and therapeutic gene delivery [150].

Moreover, the use of chitosan would facilitate the flow of particles across cellular barriers as well as opening up a narrow junction between epithelial cells [151]. Until now, this polymer has been used for coating SPIONs to produce an excellent contrast agent for MRI [152]. Hong et al. synthesised chitosan-coated ferrite nanoparticles to be studied as a contrast agent for MRI [153]. The amino groups of chitosan (–NH₂) were tied to the particles whereas the hydroxyl groups (–OH) remain untied. Consequently, these kinds of particles have slightly positively charged. Due to the existence of Coulomb repulsion between the positive charge particles and the absence of surface or organic solvents in an aqueous solution of coated particles, the solution will remain suspended in a colloidal state. Kim et al. used the sonochemical technique to produce SPIONs. Kim and their group prepared ferrofluids as a contrast agent for MRI. The nanoparticles' surface was coated with a surfactant such as oleic acid and then dispersing these particles in the chitosan [154]. These spherical particles still retained the superparamagnetic behaviour at a size of 15 nm in diameter. Microspheres composed of superparamagnetic iron oxide nanoparticles and chitosan were improved as a novel MRI-detectable embolic material. Furthermore, Lee et al. have successfully synthesised 15 nm size spherical shaped SPIONs by employing the sonochemistry process and then suspended nanoparticles within amino group chitosan to prepare a ferrofluid [155], where SPIONs/chitosan microspheres exhibited a strong improvement in MRI contrast like as ferrofluid in vitro.

2.3.2(b) Polyethylene Glycol (PEG)

PEG is a water-soluble and biocompatible polymer used in numerous applications in medicine. It is working to increase blood circulation's biocompatibility