THE FEASIBILITY STUDY OF IMPLANT MANUFACTURING USING THREE-DIMENSIONAL PRINTING AND SILICONE MOLDING

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by

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LIST OF ABBREVIATIONS

2D Two-dimensional

3D Three-dimensional

3DP Three-dimensional printing

AAOS American Academy of Orthopedic Surgeons

ABS Acrylonitrile butadiene styrene

ASTM American Society for Testing and Materials

BIS-GMA Bisphenol A-glycidyl

CAD Computer aided design

CAM Computer aided manufacturing

C-C Carbon-Carbon

CH₃ Carbon atom bonded to three hydrogen atoms

CNC Computer numerical control

Co-Cr-Mo Cobalt Chromium Molybdenum

CP-Ti Commercially pure titanium

Cr-Ni-Cr-Mo Chromium Nickel Chromium Molybdenum

CT Computer tomography

DIY Do it yourself

FDM Fused deposition modeling

HA Hydroxyapatite

Hg-Ag-Sn Mercury Silver Tin

HUSM Hospital Universiti Sains Malaysia

ISO International Standards Organization

KKTM Kolej Kemahiran Tinggi MARA

LOM Laminated object manufacturing

MJS Multiphase jet solidifications

MRI Magnetic resonance imaging

MRT Magnetic resonance tomography

MVA Motor vehicle accidents

Ni-Ti Nickel Titanium

NMR Nuclear magnetic resonance

OPSM Orthotics, prosthesis and special materials

PEEK Polyetheretherketone

PET Positron emission tomography

PET Polyethylene terephthalates

PMMA Polymethyl methacrylate

PMMA/HA HA-reinforced PMMA

PTFE Polytetra fluoroethylenes

Pt-Ir Platinum Iridium

PVC Polyvinyl chlorides

RE Reverse engineering

RM Rapid manufacturing

RP Rapid prototyping

RT Rapid tooling

RTV Room temperature vulcanizing

SERC Science and Engineering Research Centre

SGC Solid ground curing

SLM Selective laser melting

SLS Selective laser sintering

SPECT Single-photon emission computed tomography

STL Stereolithography or standard tessellation language

Ti-13Nb-13Zr Titanium Niobium13 Zirconium13

Ti-Al-Nb Titanium Aluminum Niobium

Ti-Al-V Titanium Aluminum Vanadium

Ti-Mo-Zr-Fe Titanium Molybdenum Zirconium Iron

UHMWPE Ultra high molecular weight polyethylene

UK United Kingdom

US Ultrasonic processes

USA United States of America

USB Universal serial bus

USM Universiti Sains Malaysia

UTHM Universiti Tun Hussein Onn Malaysia

UTM Universal testing machine

LIST OF SYMBOLS

% Percentage

°C Degree Celsius

σ Tensile stress

 σ_f Flexural stress

 ε Strain

μm Micrometer

 \sum Summation

 Δl Difference between original length and final length

£ Great British Pound

A Cross-sectional area

cm Centimeter

cm² Square centimeter

E Tensile Young's modulus or elastic modulus

 E_B Breaking energy

E_f Flexural Young's modulus or bending modulus

g Gram

GBP Great Britain Pound

g/cm³ Gram per cubic centimeter

h Hour

 I_s Impact strength

J Joule

J/m Joule per meter

kg Kilogram

kg/m³ Kilogram per cubic meter

kN Kilo Newton

l Final length

l₀ Original length

L Distance over which the surface deviations are measured

L Span length

m Slope of the initial straight line of stress and strain graph

ml Milliliter

mm Millimeter

mm/min Millimeter per minute

mm/s Millimeter per second

MPa Megapascal

MYR Malaysian Ringgit

N Newton

P Load applied

psi Pounds per square inch

 R_a Average roughness

USD United States Dollar

t Thickness

w Width

y Vertical deviation from nominal surface or absolute value

KAJIAN KEBOLEHLAKSANAAN PEMBUATAN IMPLAN MENGGUNAKAN PENCETAK TIGA-DIMENSI DAN PENGACUAN SILIKON

ABSTRAK

Implan telah digunakan sebagai rawatan untuk pemulihan anggota badan manusia buat sekian lama. Pada masa kini, teknologi pencetak tiga-dimensi (3DP) memberi peluang kepada proses pembuatan dalam aplikasi perubatan dan menjadi satu teknologi yang berpotensi dalam pembuatan implan. Keterbatasan prosedur pembuatan implan sekarang adalah bahan sedia ada yang digunakan dalam proses 3DP tidak diluluskan dari segi perubatan untuk implan. Selain daripada kos pembuatan yang agak tinggi, masa dan proses intensif kerja untuk mencapai model dengan kualiti yang lebih baik dalam kemasan permukaan dan ketepatan anatomi. Sifat dan ciri-ciri implan adalah sangat penting untuk dipertimbangkan. Kekasaran permukaan implan juga perlu dipertimbangkan kerana bahan digunakan mesti menyesuaikan diri dan bergabung ke dalam tisu sekeliling selepas pengimplanan. Dalam kajian ini, dua kaedah pembuatan yang berbeza, dengan menggunakan bahan serasi biologi dicadangkan sebagai alternatif yang lebih baik daripada kaedah konvensional sebelumnya bagi menghasilkan produk langsung implan dan boleh digunakan secara langsung dalam bidang perubatan. Bahan *Polymethyl methacrylate* (PMMA) telah digunakan dalam kajian ini kerana bahan ini telah biasa digunakan secara komersial dan menjadi pilihan oleh pakar bedah dalam aplikasi perubatan. Kaedah pertama yang dicadangkan ialah pembuatan langsung oleh 3DP menggunakan pencetak 3D kos rendah, yang dipanggil MakerBot Replicator. Filamen PMMA digunakan dalam kaedah ini. Kaedah kedua adalah alat pantas tidak

langsung iaitu pengacuan silikon dengan menggunakan vacuum casting. Implan dihasilkan dengan mereplikasi pola induk menggunakan pengacuan silikon di dalam ruang vakum. Selepas fabrikasi implan, analisis mengenai kajian kebolehlaksanaan antara kedua-dua kaedah fabrikasi ini di mana sifat mekanikal, sifat topologi (kekasaran permukaan), masa pembuatan dan kos pembuatan dikaji. Keputusan sifat mekanik implan yang dihasilkan oleh 3DP hampir memenuhi keperluan tulang manusia berbanding dengan implan yang dihasilkan oleh pengacuan silikon. 3DP menghasilkan kekasaran permukaan yang tinggi iaitu 6 kali lebih tinggi daripada pengacuan silikon dan mempunyai potensi untuk peratusan tinggi perlekatan sel. Berbanding dengan pengacuan silikon dan kaedah konvensional pembuatan implan, masa pembuatan oleh 3DP adalah 65% jauh lebih pendek dan kos pembuatan adalah 57% lebih rendah. Keputusan menunjukkan bahawa kedua-dua kaedah pembuatan boleh dilaksanakan dalam pembuatan implan. Namun. 3DP memberikan lebih banyak kelebihan dan menjadikannya lebih mudah untuk digunakan dalam pembuatan implan dan fabrikasinya dengan mengambil kira kos, masa dan manfaat daripada pembuatan implan yang disesuaikan untuk pesakit tertentu. 3DP boleh membuka jalan untuk teknologi yang lebih canggih dan memberi sumbangan besar dalam bidang perubatan.

Kata kunci:

Aplikasi perubatan; Implan perubatan; Pencetak tiga-dimensi; *MakerBot Replicator*; Pengacuan silicon; *Vacuum casting*; PMMA; Sifat mekanikal; Sifat topologi; Masa pembuatan; Kos pembuatan.

THE FEASIBILITY STUDY OF IMPLANT MANUFACTURING USING THREE-DIMENSIONAL PRINTING AND SILICONE MOLDING

ABSTRACT

Implant has been used as a treatment for the restoration of the human body for a long time. Nowadays, three-dimensional printing (3DP) technology provides opportunity to the manufacturing process in medical applications and become a potential technology in implant manufacturing. The limitation of the current implant manufacturing procedure is the existing materials used in 3DP process are not medically approved for implant. Apart from relatively high production cost, time and work intensive process to achieve model with better quality in surface finish and anatomical accuracy. The properties and the characteristics of the implant are very important to be considered. The surface roughness of the implant needs to be considered as the material must adapt to and blend into the surrounding tissue after implantation. In this research, two different manufacturing methods by using biocompatible material are proposed as improved alternative of the previous conventional method in order to produce direct product of implant and can be used directly in medical field. Polymethyl methacrylate (PMMA) material used in this study as the material is already commercially established and most preferred by surgeons in medical application. First proposed method is direct production by 3DP using a low cost 3D printer, called MakerBot Replicator. PMMA filament was used in this method. The second method is indirect rapid tooling (RT) which is silicone molding by using vacuum casting. The implant was produced by replicating the master pattern using silicone molding under vacuum chamber. After the implant fabrication, the analysis on the feasibility study between both fabrication methods in

which mechanical properties, topological properties (surface roughness), production time and production cost were investigated. The results of mechanical properties of implant produced by 3DP barely meet human bone requirement as compared to implant produced by silicone molding. 3DP produces high surface roughness which is 6 times higher than silicone molding and has potential for high percentage of cell attachment. As compared to the silicone molding and the conventional method of implant manufacturing, the production time by 3DP is 65% much shorter and the production cost is 57% lower. The results show that both manufacturing methods are feasible to apply in implant manufacturing. However, 3DP provides more advantages and make it more feasible to apply in implant manufacturing and fabrication taking into accounts the cost, time and benefit of highly customized implant for specific patient. 3DP can pave the ways to more advanced technology and gives great contribution to the medical field.

Keywords:

Medical application; Medical implant; Three-dimensional printing; MakerBot Replicator; Silicone molding; Vacuum casting; PMMA; Mechanical properties; Topological properties; Production time; Production cost.

CHAPTER ONE

INTRODUCTION

1.1 Introduction

This chapter consists of six sections which provide general ideas of this research. First section is research background which contains theoretical foundations related to the research and elaboration of research planning. Second section is problem statements and next is research objectives. Then, research hypotheses, scope of research and thesis outlines are illustrated in this chapter.

1.2 Research background

In many medical cases where implant is needed, it is common practice traditionally, to produce implant by cutting metal pieces, usually stainless steel or Titanium, or sometimes bovine bones to be fitted into patients in place of damaged bones, as temporary bridging structure or permanent replacement. The conventional techniques where traditional fabrication like sawing, cutting or bending in the workshop to fit varying patient sizes are time consuming and in only roughly estimated dimensions. This often created misfit on patients, leading to problem like premature implant loosening and excessive wear over a period of time leading to prolong uncomfortable living for patient. Implant cannot be easily and accurately customized according to unique size and lifestyle of individual patient. The recent development manufacturing technology, namely three-dimensional printing (3DP) offers the opportunity to improve medical implant fabrication.

3DP technology is a promising and powerful technology that can potentially improve and revolutionized field of medical science (Bagaria *et al.*, 2011b). 3DP technology

can fabricate models with complex geometric forms, making it very suitable for reproducing the intricate of the human body (Raos *et al.*, 2005). By conventional method of casting or handcrafting, the fabrication of customized implants to fit everyone is challenging and in many cases, it is impractical to accomplish because of high cost and tight timeline (Frank *et al.*, 2008). By using layer-based nature of 3DP technologies, the creation of complex freeform shapes is very feasible, hence allowing customization to fit each patient.

The manufacturing of medical models such as implant using 3DP technology begins with the acquisition of three dimensional shape data of both internal and external human body structures using medical scanners such as Computer Tomography (CT) and Magnetic Resonance Tomography (MRT), which are commonly used in medical imaging to obtain anatomical information. The data from medical imaging is then used for the production of 3D physical object by using CAD/CAM system, in a 3DP apparatus. Although 3DP technology has been around since the last 15 years, it is relatively new in medical field. The use of 3DP in medical is not satisfactorily high, despite the potential benefits.

Implant is used as treatment for the restoration of the human body that has been lost due to traumatic injuries and non-traumatic events. In recent years, some of the biomaterial used in implant manufacturing to fill the defect includes bioceramics, biopolymers, metal and composites. Titanium and polymeric materials such as polymethyl methacrylate (PMMA) and polyetheretherketone (PEEK) are the most preferred by surgeons in medical applications because of their excellent mechanical properties and biocompatibility (Rahim *et al.*, 2015b). Most implants are just simple models that only give approximate fit to the patients. By referring to the previous and recent studies, the material of polymethyl methacrylate, (PMMA) was proposed in

this research. This is because PMMA material is already established and mostly used in medical implant by researcher from previous and recent studies (Teo *et al.*, 2016).

A research on biocompatible implant manufacturing was carried out, including the analysis of the PMMA material as potential material for implant. The proposed solutions of implant manufacturing process are divided into two different processes; direct printing using 3DP and indirect production using Rapid Tooling (RT). In direct printing using 3DP, implant material must be printable and also biocompatible. A low cost 3DP machine (MakerBot Replicator 2X) based on fused deposition technology where solid filament is fused, was used in 3D printing. For indirect implant fabrication using rapid tooling, silicone molding was used where a 3D physical model of the implant (also known as the master pattern) from any material is first produced using 3D printer, then used in subsequent silicone molding process to replicate the implant in the form of actual biocompatible material. The feasibility of the two methods for implant manufacturing is assessed based on the results of analysis in characterization of material, topological properties, production time and production cost.

1.3 Problem statements

There are 6.3 million fractures each year in the United States, according to the AAOS (American Academy of Orthopedic Surgeons). In addition, the costs associated with these fractures are extremely expensive. In fact, there were more than 500,000 bone graft procedures performed in the USA in 2005 and charged about USD 2.5 billion (Stevens *et al.*, 2008). That means the costs related to the fractures are too expensive. In medical data reported in Hospital Universiti Sains Malaysia (HUSM) between 2007 and 2011, 447 patients had experienced maxillofacial (jaws

and face region) fractures (Pohchi *et al.*, 2013). 85% of the maxillofacial fractures were caused by the motor vehicle accidents (MVA) and followed by falls (5%), fight and assaults (4%), sports related injuries (3%), industrial accidents (2%) and others (1%). This showed MVA was the main factor of the maxillofacial fractures reported in HUSM.

In early implant production, the conventional manufacturing procedures are milling, casting and injection molding (Raos *et al.*, 2005). Milling can be used to produce surgical instruments with low material cost (Petzold *et al.*, 1999). Implant production cost by milling is lower than in the 3DP process (Raos *et al.*, 2005). However, the geometric accuracy is poor, which is (±1.5 mm) (Petzold *et al.*, 1999). Before this, modifying implants into a desired shape, size and fits should be done by shaving pieces of metal and plastic using scalpels and drills or sometimes surgeons need to perform bone graft surgeries (Ventola, 2014), which can be time consuming for the whole process of implant production.

Nowadays, the use of 3DP technology in medicine is already known. Unfortunately, it is not satisfactory high since it is a relatively young field, and has wide potentials to be reached (Silva *et al.*, 2014). Currently in Malaysia, the craniofacial implant that used by oral maxillofacial surgeon is mostly imported from overseas and the cost can be varies depends on the material, size and complexity of defects, but generally very high. In medical, CT scan or MRT are commonly used imaging techniques for diagnostic purpose before medical team and the patient can decide the next best treatment. CT and MRT data are only 2D virtual images of different layers of patient's anatomy, as such are difficult to comprehend. With 3DP, such 2D data may be printed in 3D physical form allowing for better assessment of the disease. This can be extended to implant design and fabrication where CT or MRT data can be