DESIGN OF EXPERIMENT (DOE) STUDY OF HYDROXYAPATITE (HA) FOR LOAD BEARING APPLICATION VIA $\mathbf{2}^k$ FACTORIAL DESIGN

by

NURUL SHAFYRA BINTI MOHD SABRI

Thesis submitted in fulfillment of the requirements

For the degree of

Master of Science

UNIVERSITI SAINS MALAYSIA

AUGUST 2013

DECLARATION

I hereby declare that I am the sole author of this dissertation. This is a through copy of

the dissertation, including any required final revisions, as accepted by my examiners. It

has not previously submitted for the basis of the award of any degree or diploma or

other similar title of this for any other diploma/examining body or university. I

understand that my dissertation may be made electronically available to the public.

Name of student : Nurul Shafyra b

: Nurul Shafyra bt Mohd Sabri

Signature:

Date

Witnessed by

Supervisor : Dr. Shah Rizal b. Kasim

Signature:

Date

ii

ACKNOWLEDGEMENT

First of all I thank ALLAH, who bestowed me with the strength to complete this work.

There were a great number of people who helped make this journey possible. Foremost, I would like to express my sincere gratitude to my supervisor, Dr. Shah Rizal Kasim, of the School of Material and Mineral Resources Engineering, Universiti Sains Malaysia for his relentless encouragement, constructive guidance and words of motivation throughout the duration of this research study and moreover for the inspiration he provided to ensure the completion of this work. His expertise, availability to discuss ideas and willingness to give of his knowledge were instrumental. For this, I will be eternally grateful.

I would also like to express my gratitude to my co-supervisor, Prof. Ahmad Fauzi Mohd Noor, for his guidance and helpful opinion during this research. Unforgettably, I am also thankful to Dean, Deputy Dean and all the lecturers. A special word of thanks also goes to all the staffs and technicians of School of Material and Mineral Resources Engineering for their technical support and assistance.

Last but not least, I would like to express my thanks to my parents, Mohd Sabri Md. Noor and Che Embon Idris for all their heartfelt prayers. And especially to my sisters, brothers, friends and colleagues for all their good wishes of encouragement and support over the last few months, which will always be remembered with deep gratitude.

TABLE OF CONTENTS

TITI	TITLE		
AUTHOR'S DECLARATION			ii
ACK	ACKNOWLEDGEMENT		
TAB	LE OF CONTENTS		iv
LIST OF TABLES			viii
LIST	OF FIGURES		ix
LIST	OF ABREVIATION		xii
ABS	ABSTRAK		
ABS	ABSTRACT		
СНА	PTER ONE: INTRODUCTION		
1.1	Background		1
1.2	Problem statement		3
1.3	Research Objectives		6
1.4	Research Approach		6
СНА	PTER TWO: LITERATURE REVIEW		
2.1	Introduction		8
2.2	Desired Properties of Implantable Biomaterials		8
2.3	Bioceramics		10
2.4	Application of Bioceramics		11

2.5	Biological Apatite		12
	2.5.1	Natural Human Bone Mineral	12
	2.5.2	Mechanical Properties Of Human Bone	19
2.6	Hydro	oxyapatite	20
	2.6.1	Introduction	20
	2.6.2	Mechanical Properties of HA	22
	2.6.3	Thermal Effects on HA	24
		2.6.3.1 Sintering Process	24
		2.6.3.2 Thermal Stability of HA	26
		2.6.3.3 Factors Affecting Thermal Decomposition Of HAp	29
		2.6.3.3(a) Sintering Temperature and Atmosphere	29
		2.6.3.3(b) Ca/P Molar Ratio	31
		2.6.3.3(c) Initial Particle Size	32
		2.6.3.3(d) Initial HA Synthesis Reaction	33
		2.6.3.3(e) Secondary Phases	33
2.7	HA ba	ased Biocomposite	33
2.8	Alum	umina	
2.9	Design of Experiment (DOE) of HA/Al ₂ O ₃ Biocomposite		36
	2.9.1	DOE Approach	36
	2.9.2	DOE via 2-Level (2 ^k) Factorial Design	37
	2.9.3	Analysis of Variance (ANOVA)	38

CHAPTER 3: METHODOLOGY

3.1	Introduction		39
3.2	PART I		
	3.2.1	Raw materials	40
	3.2.2	HA/Al ₂ O ₃ Biocomposite Preparation	41
		3.2.2.1 Batching and Powder Mixing	43
		3.2.2.2 Drying and Sieving	43
		3.2.2.3 Uniaxial Pressing	43
		3.2.2.4 Sintering Process	44
	3.2.3	Characterization of the HA/Al ₂ O ₃ Biocomposite	44
		3.2.3.1 X-ray Diffraction (XRD)	45
		3.2.3.2 Field Emission Scanning Electron Microscopy (FESEM)	46
		3.2.3.3 Particle Size Analysis	46
		3.2.3.4 Density and Porosity Measurement	47
		3.2.3.5 Hardness Testing	48
3.3	Part II	: Design of Experiment (DOE) via 2 ^k Factorial Design	49
	3.3.1	State Objectives	51
	3.3.2	Response Variables Selection	51
	3.3.3	Input Factors Selection	52
	3.3.4	Design Selection	52
	3.3.5	Strategy Development : Randomization	53
	3.3.6	Run Experiment	54
	3.3.7	Model interpretation	55

		3.3.7(a) Regression model	56
		3.3.7(b) Analysis of Variance (ANOVA)	56
		3.3.7(c) Residual Analysis	56
		3.3.7(d) Interaction effects	57
		3.3.7(e) 2-D Contour Plot and 3-D Surface Plot	57
СНА	PTER 4	4: RESULT AND DISCUSSION	
4.1	Introd	luction	58
4.2	Part I	: Characterization of Raw Material	59
	4.2.1	Particle Size Analysis	59
	4.2.2	Powder Morphology	60
	4.2.3	Elemental Analysis	62
	4.2.4	X-Ray Diffraction Analysis (XRD)	63
4.3	Part I	I: Screening through 2 ^k Factorial Design	64
	4.3.1	Model Development: Hardness Response	66
		4.3.1.1:The Effects of Al ₂ O ₃ Composition variation on the	
		Hardness Response	75
		4.3.1.2:The Effects of Sintering Temperature Variation on the	
		Hardness Response	76
	4.3.2	Model Development: Porosity Response	79
	4.3.3	Model Development: Density Response	87
		4.3.3.1 Effects of Sintering Temperature Variation on the	
		Porosity and Density Response.	96

	4.3.3.	2 Effects of Al ₂ O ₃ Composition Variation on the Density	
		and Porosity Response	99
СНА	PTER 5: CON	ICLUSION	
5.1	Conclusion		101
5.2	Recommenda	ation for Future Research	103
REFI	REFERENCES		
APPI	ENDICES		
APPE	ENDIX A	ICSD Card	112
APPE	ENDIX B	Main and Interaction Effects Summary	135

LIST OF TABLES

		Page
2.1	Bioceramics and its application	12
2.2	Composition of the mineral phase in human bone	15
2.3	Mechanical properties of a compact human bone	19
2.4	Some Calcium Phosphate Compounds	21
2.5	Physical properties of synthetic HA	23
2.6	Mechanical properties of synthetic HA	23
2.7	The reaction of HA corresponding to the heating temperature range	28
2.8	Mechanical properties of biomedical grade Al ₂ O ₃	36
2.9	Summary of DOE studies of HA/Al ₂ O ₃ biocomposite	38
3.1	Summary of raw materials used for HA/Al ₂ O ₃ biocomposite	41
3.2	Experimental factors and levels of factors	53
3.3	Experimental design matrix	54
4.1	The design layout of 2 ^k factorial design	65
4.2	Analysis of variance (ANOVA) for the models derived from 2 ^k	
	factorial of HA hardness as the response	70
4.3	Estimation of the linear model of level factorials (coded unit)	71
4.4	Type of effect based on regression analysis	72
4.5	Analysis of variance (ANOVA) for the models derived from 2 ^k	
	factorial of HA porosity as the response	83
4.6	Estimation of the linear model of level factorials (coded unit)	84
4.7	Type of effect based on regression analysis	84
4.8	Analysis of variance (ANOVA) for the models derived from 2 ^k	
	factorial of HA density as the response	92
4.9	Estimation of the linear model of level factorials (coded unit)	93
4.10	Type of effect based on regression analysis	93

LIST OF FIGURES

		Page
2.1	Chemical compositional analysis of human bone	13
2.2	Compartment of bone tissue (Martin et al. 1998)	14
2.3	The structure of bone	17
2.4	The bone remodeling cycle	18
2.5	Phase diagram of the system CaO-P2O5 at high temperature.	
	No water present	30
2.6	Phase diagram of the system CaO-P ₂ O ₅ at high temperature;	
	at a partial water pressure of 500mmHg	31
3.1	Flow chart of HA/Al ₂ O ₃ biocomposite preparation	
	and characterization	42
3.2	Schematic illustration of the density measurement using Archimedes	
	Principle	47
3.3	Schematic of diamond indentation mark	48
3.4	General framework of 2 ^k factorial design	50
4.1	Particle size distribution curve for (a) HA powder and	
	(b) Al ₂ O ₃ powder	60
4.2	Morphology of HA powder	61
4.3	Morpholgy of Al ₂ O ₃ powder	62
4.4	SEM and EDX spectrum of HA powder	63
4.5	Comparison of HA diffraction pattern with HA database	64
4.6	Normal plot of the standardized effect for parameters studied where	
	response is hardness (alpha = 0.05)	69
4.7	Residual plot on hardness response data based on regression model	73
4.8	2-D contour plot and 3-D surface plot in response to hardness result	74
4.9	The diffractrogram of HA/Al ₂ O ₃ biocomposite (0 and 30 wt%	
	respectively) sintered at 1250 °C	77
4.10	The diffractrogram of HA/Al_2O_3 biocomposite sintered at $1100^{\circ}C$	
	and 1250°C	78

4.11	Normal plot of the standardized effect for parameters studied where		
	response is porosity (alpha = 0.05)	82	
4.12	Residual plot of actual and predicted experimental data based		
	on regression model	85	
4.13	(a)2-D contour plot corresponding to porosity results	86	
4.13	(b)3-D surface plot corresponding to porosity results	87	
4.14	Normal plot of the standardized effect for parameters studied where		
	response is density (alpha = 0.05)	90	
4.15	Scatter diagrams of relationship between actual and predicted		
	experimental data based on regression model	94	
4.16	(a) 2-D contour plot corresponding to density results	95	
4.16	(b)3-D surface plot corresponding to density results	96	
4.17	FESEM of hydroxyapatite (HA) at different sintering temperature;		
	a)1100°C, b) 1150°C and c) 1250 °C at 0 wt% Al ₂ O ₃	98	
4.18	FESEM of hydroxyapatite (HA) at different amount of Al ₂ O ₃		
	a) 0 wt% and b) 30 wt% at 1250 °C sintering temperature	100	

LIST OF ABREVIATIONS

2-D 2 Dimension

2^k Two Level

3-D 3 Dimension

ACP Amorphous Calcium Phosphate

Al₂O₃ Alumina

ANOVA Analysis of Variance

Ca/P Calcium to Phosphate Ratio

 $Ca_{10}(PO_4)_6(OH)_2$ Hydroxyapatite

Ca²⁺ Calcium

CaO Calcium Oxide

CDA Calcium Deficient Apetite

Cl⁻ Chloride

ClA Chlorapatite

CO₃²- Carbonate

DOE Design of Experiment

EDX Energy Dispersive X-ray Spectroscopy

F Fluoride

FA Fluorapatite

FESEM Field Emission Scanning Electron Microscopy

GPa Gigapascal

HA Hydroxyapatite

HA/Al₂O₃ Hydroxyapatite Reinforced with Alumina

HIP Hot Isostatic Pressing

ICSD International Centre of Structural Data

K⁺ Potassium

 $K_{\rm IC}$ Fracture Toughness

Mg²⁺ Magnesium MPa Megapascal

Na⁺ Sodium

P Phosphate

PSZ Partially stabilized zirconia

 $\begin{array}{ccc} R^2 & & R\text{-square} \\ R^2_{adj} & & R \text{ adjusted} \\ R^2_{pred} & & R \text{ predicted} \end{array}$

S/N Signal to Noise Ratio

SEM Scanning Electron Microscopy

SiC Silicon Carbide

TCP Tricalcium Phosphate

TTCP Tetracalcium Phosphate

XRD X-ray Diffraction

Y₂O₃ Yttrium oxide

ZrO₂ Zirconia

 $\alpha ext{-}$ TCP Alpha- Tricalcium Phosphate $\beta ext{-}$ TCP Beta- Tricalcium Phosphate

 $\lambda \hspace{1cm} Wavelength$

KAJIAN REKABENTUK EKSPERIMEN (DOE) TERHADAP HIDROKSIAPATIT UNTUK APLIKASI PENGALAS BEBAN MENERUSI KAEDAH FAKTORAN 2^k

ABSTRAK

Tujuan kajian ini adalah untuk menghasilkan biokomposit hidroksiapatit (HA)/alumina (Al₂O₃) dengan menggunakan kaedah percampuran kering bagi mengkaji faktor eksperimen dan kesannya (kesan utama dan kesan interaksi) terhadap sifat akhir biokomposit (kekerasan, ketumpatan dan keliangan). Kesan-kesan ini diukur menggunakan rekabentuk eksperimen (DOE) bagi membentuk model matematik. Kajian ini merangkumi dua bahagian di mana bahagian I adalah berkaitan dengan caracara penyediaan sampel yang bermula dengan pencirian sifat fizikal, struktur (fasa) dan sifat kimia bagi bahan mentah. Prosedur ini diikuti dengan fabrikasi biokomposit HA/Al₂O₃ berdasarkan parameter yang berbeza (suhu pensinteran ;1100 °C dan 1250 °C, masa pencampuran ; 3 jam dan 9 jam dan komposisi Al₂O₃; 0wt% dan 30 wt%). Eksperimen ini dijalankan mengikut turutan yang dicadangkan oleh perisian DOE (Minitab 16) semasa proses perawakan. Setelah itu, sifat fizikal dicirikan melalui ujian ketumpatan dan keliangan manakala morfologi sampel dilihat dengan menggunakan mikroskop imbasan elektron (SEM). Bagi analisis fasa,sampel dicirikan menggunakan analisis pembelauan sinaran-X (XRD) dan ujian kekerasan Vickers digunakan untuk mengkaji kekerasan sampel. Dalam bahagian II, kaedah DOE faktoran dua aras (2^k) untuk mengkaji faktor-faktor yang memberi kesan dalam digunakan penghasilan biokomposit HA/Al₂O₃ berkekuatan tinggi. Faktor-faktor ini dianalisis dan faktor yang memberi kesan besar ditentukan menerusi model regresi dan analisis variasi (ANOVA). Model disahkan menerusi ANOVA bagi mengkaji kepadanan antara model

dan data yang diperoleh secara eksperimen. Seterusnya, ralat eksperimen dan interaksi antara parameter dikaji untuk mengenalpasti perbezaan antara nilai data ramalan dan data eksperimen. Keputusan menunjukkan komposisi Al₂O₃ dan suhu pensinteran telah memberi kesan yang besar ke atas respon manakala masa pencampuran tidak memberikan sebarang pengaruh. Untuk respon kekerasan, analisis telah menunjukkan bahawa untuk mendapatkan kekerasan yang tinggi, suhu pensinteran haruslah ditetapkan di atas suhu 1240 °C dan komposisi Al₂O₃ haruslah berada di bawah 3 wt%. Syarat yang sama juga diperlukan bagi respon keliangan di mana suhu pensinteran haruslah ditingkatkan melebihi 1188 °C dan komposisi Al₂O₃ haruslah berada di bawah 7 wt% untuk mendapatkan keliangan antara 5-10 %. Bagi respon ketumpatan, ketumpatan yang hampir menyamai ketumpatan tulang manusia (lelaki : 3.88 g/cm³; wanita : 2.90 g/cm³) boleh diperolehi dengan menetapkan suhu pensinteran masing-masing pada 1180 °C ke atas dan komposisi Al₂O₃ dibawah 30 wt% atau suhu pensinteran pada 1200 °C ke atas dan komposisi Al₂O₃ melebihi 10 wt%. . Secara keseluruhan, parameter yang memberi kesan besar terhadap respon-respon adalah komposisi Al₂O₃ dan suhu pensinteran.

DESIGN OF EXPERIMENT (DOE) STUDY OF HYDROXYAPATITE (HA) FOR LOAD BEARING APPLICATION VIA 2^k FACTORIAL DESIGN

ABSTRACT

The present study aims to fabricate hydroxyapatite (HA)/alumina (Al₂O₃) biocomposite via dry mixing process, in order to evaluate the experimental factors and their effects (main effects and interaction effects) on the response or final biocomposite characteristics (hardness, density, and porosity). These effects were quantified using Design of Experiments (DOE) to develop mathematical models. This study covered two parts where the part I deals with the sample preparation procedures which was started with the characterization of raw materials in term of physical, structural (phases) and chemical properties. This procedure was followed by the fabrication of HA/Al₂O₃ biocomposite with different parameter setting (sintering temperature; 1100 °C and 1250 °C, mixing time; 3 hours and 9 hours and Al₂O₃ composition; 0wt% and 30 wt%). The experiment was run by following the run order suggested by DOE software (Minitab 16) through randomization stage. Next, the physical properties was characterized using density and porosity testing while the morphology of the sample was studied using Scanning Electron Microscopy (SEM). For phase analysis, the sample was characterized through X-ray Diffraction analysis and Vickers hardness testing was employed to study its hardness. In part II, two-level (2k) factorial method of DOE was employed to determine the suitable or significant factors in producing high strength HA/Al₂O₃ biocomposite. The experimental factors were analyzed and the significant factors were

determined through regression model and Analysis of Variance (ANOVA). The model was then validated through ANOVA in order to study how fit is the model with the experimentally obtained data. Experimental errors and interactions between factors were investigated to verify the significant between predicted and experimental data. Results shows that Al₂O₃ composition and sintering temperature has given a significant effects on the responses while mixing time has given no influence. For hardness response, it shows that, in order to obtained a high hardness, the sintering temperature must be set above 1240 °C with Al₂O₃ composition lower than 3 wt%. The same requirement goes to porosity response where sintering temperature must be above 1188 °C with Al₂O₃ composition below 7 wt% in order to obtained 5-10 % porosity. For density response, acceptable density that mimicking the natural dense male and female bone density (3.88 g/cm³ for male; 2.90 g/cm³ for female) can be obtained by setting the sintering temperature above 1180 °C and Al₂O₃ composition below 30 wt% or sintering temperature above 1200 °C and Al₂O₃ composition above 10wt % respectively. The most significant parameters that effecting all the response are Al₂O₃ composition and sintering temperature.

CHAPTER 1

INTRODUCTION

1.1 Background

Medical world is in a transition where damaged organ is completely replaced with in vitro synthesized implants instead of curing it by lengthy surgical operations (Grained, 2011). However, only a few materials are known to satisfy the requirements of implantation in the human body. For example, materials such as vanadium steel, which was chosen for its good mechanical properties has corroded rapidly in the body and had caused infection or adverse effects on the healing process (Raynaud et al., 2002). However, these drawbacks regarding the infections and adverse effects tend to be solved by the application of biocompatible materials known as biomaterials (Mizuno, 2007).

Biomaterials can be simply defined as a synthetic materials used to replace part of a living system or to function in intimate contact with living tissue (Hench, 1991). It is considered clinically success when it has stable interface between implant and connective tissues, excellent resistance to corrosion, noncarcinogenic, acceptable to cyclic loading, high wear resistance and have a biocompatible chemical composition to avoid adverse tissue reaction (Best et al., 2008).

One of the attractive biomaterials is bioceramic where it can be classified into bioinert, bioactive and resorbable bioceramics (Hench, 1991). The selections of bioceramics are depends on its application. For instance, hard tissue and bone replacements are synthesized mainly from bioactive ceramics such as dense non-porous bioglass, ceravital and hydroxyapatite, (HA) (Best et al., 2008). However, in this application, HA has dominated any other material in quantity primarily because of its compositional and biological similarity to human bone, biocompatibility, bioactivity and osteoconduction characteristic (Jun et al., 2003).

Even though HA offers high biocompatibility, relatively low density, high compressive strength and high hardness, application of HA as a load bearing implant is limited because of its brittleness, relatively low-mechanical properties and a high-dissolution rate in body fluid. Hence, arise the need to reinforce the HA without hampering its biocompatibility (Balani et al., 2007)

Introduction of bioinert ceramics with better properties into HA ceramic is the effective way in producing a composite with acceptable strength in order to sustain the cylic loading (Mizuno, 2007). Bioinert ceramics are chosen to enhance the properties of bioactive HA because it can maintain their physical and mechanical properties while being implant in human body. Examples of bioinert ceramics are alumina, (Al₂O₃), zirconia, (ZrO₂), and carbons (Piconi and Maccauro, 1999).

1.2 Problem statement

Hydroxyapatite (HA) is a calcium phosphate bioactive material. It posses excellent biocompatibility, good osteoconduction properties (allow bone cells to grow on its surface) and identical chemical composition to the mineral phase of human bones (Shahriar, 2009). The benefits of HA as implants material have been widely acknowledged, but the occurrence of several poor performances such brittleness, relatively low-mechanical properties and high dissolution rate has generated concerns over the improvement of monolithic HA properties (Gergely et al., 2010).

The addition of zirconia, (ZrO₂) was proven to improve mechanical properties of HA such as fracture toughness and hardness (Piconi and Maccauro, 1999). However, the addition of ZrO₂ has led to a large volume change since it is not stable at high temperature. Thus, an adequate amount of dopant such as yttrium oxide (Y₂O₃) is used to stabilize the ZrO₂ properties at elevated temperature (Firmandika, 2008). ZrO₂ produced in this manner is referred as partially stabilized zirconia, (PSZ). Since the addition of ZrO₂ to HA involves multi steps preparation method, it requires a lot of time, thus making the process become even more costly (Piconi and Maccauro, 1999). Another attempt that has been done to enhanced the HA based composite properties is by adding silicon carbide, (SiC) (Hench 1991). Addition of SiC does not favor a high cost compared to PSZ but due to toxicity issues, the use of this material as biological implant has became restricted (Mizuno, 2007). Therefore, finding the suitable materials that are non toxic and cost effective is a must.

Alumina (Al_2O_3), being a bioinert material, has shown much promise. It posses high hardness, thus leads it to have the tribologic advantage (Jun et al., 2003). This properties is

one of the focus in the fabrication of load-bearing implant in order to prevent wear-debris generation since it might cause adverse affect to the human body (Hench, 1991). Since Al_2O_3 is a bioinert ceramic, it offers excellent degradation resistance and has biocompatible chemical composition which can avoid adverse tissue reaction (Grained, 2011). In addition, Al_2O_3 is insoluble in all ordinary chemical reagents which allow it to be planted in human body environment (Best et al., 2008). These qualities have make Al_2O_3 useful as a biomaterial.

Other than restriction in choosing a suitable reinforcement material, the complex procedures and high cost in HA based biocomposite fabrication has becoming another issue. HA based biocomposite are mainly produced by using heterogenous precipitation and wet mixing method (Grained, 2011). These methods are time consuming since it involved a lengthy homogenization, stirring and drying process. Moreover, the pH need to be monitored thoroughly during the precipitation process until it was done (Epure et al., 2007). The usage of hot isostatic pressing (HIP) also can enhance the composite mechanical properties (Adolfsson et al., 2000). However, all these fabrication processes demand high cost and time which most researchers or manufacturers try to refrain.

With this background, it shows that the fabrication of biocomposite need to take account the biocompatibility, strength and cost. Conversely, the key of success of any implant, besides the correct surgical implantation, is the strict quality control during fabrication of the materials and the production of the implant (Hench, 1991). There are many factors affecting the quality and technical performances of the processing during the production, such as raw material selection, and process set up (N. Al et al., 1998). Trial and

error method or conventional research methodology are frequently used to determine the optimal process parameters. This definitely involving a high cost and consuming a lot of time since a lot of experiment need to be done. Conventional methodology will generate a number of tests which do not always lead to conclusive and effective results (Kehoe and Eng, 2008). In order to reduce the frequency of experiment and determine factors influencing the characteristic of the product, Design of Experiment, (DOE) method can be adopted (Cabrelon and Zauberas 2008). In short, DOE mathematical models can be used to quantify the experimental output effectively and economically (Rajalingam et al., 2012).

The usage of DOE in determining the optimal process setting of HA/Al₂O₃ biocomposite fabrication has not been excessively done in the literature. Thus, the potential parameters or predictors (sintering temperature, mixing time and Al₂O₃ composition) that might influence the mechanical properties of the biocomposite will be studied by using this approach. The suitability of low cost conventional dry mixing process in HA/Al₂O₃ biocomposite fabrication also will be investigated based on the results obtained.

In this study, the DOE was carried out by using statistical tool known as two-level (2^k) factorial design which is widely used for experiment that involving several factors for a response. Factorial design is a combination of mathematical and statistical techniques which used in the modeling and analyzing of problems to get an improved response (Klimova et al., 2006). The interactions or relationships between inputs factors and one or more measured factors also can be quantified by using this tool. Since the levels involves in this study is only 2-levels, 2^k factorial design was chosen. In addition, another advantage of

2^k factorials are widely used in research work is because they are capable to form basis experimental design with considerable practical value.

1.3 Research Objectives

There are two main objectives for this research work:

- 1) To use Design of Experiment (DOE) method to determine the significant parameters among the predictors (sintering temperature, mixing time and Al₂O₃ composition) on the resultant mechanical properties of HA/Al₂O₃ biocomposite.
- 2) To study the usage reliability of dry mixing process whether it can improve the monolithic HA properties as those researches that used the complex and cost demanding process.

1.4 Research Approach

To achieve the mentioned objectives, research experimental investigations were divided into two main parts as follows:

Part I: This part deals with the preparation procedures which was started with the characterization of raw materials. Physical and chemical properties of commercial HA and Al₂O₃ powders were characterized. This procedure was followed by the fabrication of HA/Al₂O₃ biocomposite with different parameter setting (sintering temperature; 1100 °C and 1250 °C, mixing time; 3 hours and 9 hours and Al₂O₃ composition; 0wt% and 30 wt%). The

experiment order was set by the Design of Experiment (DOE) through randomization stage. Physical, structural and hardness properties of this biocomposite were then characterized using X-ray Diffraction analysis (XRD), Scanning Electron Microscopy (SEM), density and porosity testing as well as Vickers hardness testing.

Part II:

DOE via two-level factorial method was employed to determine the suitable or significant factors in producing high strength of HA/Al₂O₃ biocomposite. The experimental predictors or parameters (mixing time, sintering temperature and Al₂O₃ composition) were analyzed and the significant factors (factors that affecting the process and output) were determined through regression model. The model was then validated through mean square, (R²) and mean square adjusted, (R² adjusted) observation in order to study how fit is the model with the obtained data. This approach was followed by the evaluation of experimental errors and interactions between parameters to study the correlations between each factors investigated. The characterization of the prepared samples based on the run order arrangements suggested by randomization process has been discussed to support the DOE results and useful in generating inference.

These two parts were studied, compared and evaluated to distinguish which parameter is giving significant effects to the hardness properties of HA/Al_2O_3 biocomposite.